Eye-Lens Dose Reduction using Region of Interest (ROI) Attenuators in Neuroimaging

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INTRODUCTION

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- > Cataracts and opacities could result following the exposure of the eye lens to radiation above a threshold dose.¹
- > The International Commission on Radiological Protection (ICRP) has determined a cataractogenesis threshold value to 0.5 Gy, a reduction below the previous threshold of 5 Gy.²
- \succ In neuro-imaging procedures, primary focus is on the region of interest (ROI) containing the pathology, which requires detailed information needed for diagnosis and procedural guidance,



Figure 5: Lateral projection showing the combination of the small and large square FOV's to simulate the ROI attenuator exposure on the Zubal computational phantom.

 \succ The dose to the eye lens per entrance air kerma with the ROI attenuator (LD_{ROI}) can be estimated as:

 $LD_{ROI} = \{f \times LD_{L} + (1-f) \times LD_{S}\}....(1)$

where f, transmission factor, is the fraction of the beam exposure transmitted by the attenuator.



whereas a lower-quality image could be acceptable in the periphery, which is primarily used for reference.³⁻⁴

- > Use of an attenuator with a hole for the ROI as shown in Figure 1 reduces dose in the attenuated region, while allowing reference features to be seen.
- \succ Equalization of the image brightness in the periphery to that in the ROI can be achieved by use of a Convolutional Network Neural (CNN),⁵ which produces an ROIboundary artifact-free, full-field image with equalized brightness and noise as seen in Figure 2.



Figure.1 ROI imaging showing beam attenuator with round ROI aperture.

 \succ This study estimated the dose reduction to the eye lens using ROI attenuators of varying transmission factor as a function of gantry angulation and head shift from isocenter.



- > The percent lens-dose reduction relative to the full field dose without attenuator is given as:

 $LDR = 100 \times \{LD_{I} - LD_{ROI}\}/LD_{I}$

RESULTS

Note 1: The Zubal computational head is tilted such that the eyes are not symmetrically centered but shifted by about 1 cm to the right of the phantom centerline as seen in Fig. 6 where the lenses are depicted by red pixels on the head. Note 2: The beam dimensions in Figures 6-10 are not to scale.



Figure 6: (A) Axial cross section showing head centered on the isocenter and the ROI attenuated beam for lateral and PA projections. (B) % LDR for right (R) and left (L) lens as a function of LAO gantry angle for different transmission factors with 0cm head shift from isocenter.

Figure 9: (A) Sagittal cross section showing head shift in the -y direction and the ROI attenuated beam for PA projection. (B) % LDR for right (R) and left (L) lens as a function of LAO gantry angle for different transmission factors (f) for a head shift from isocenter of -4 cm in the cranial direction.



Figure 10: (A) Sagittal cross section showing head shift in the +y direction and ROI attenuated beam for PA projection. (B) % LDR for right (R) and left (L) lens as a function of LAO gantry angle for different transmission factors for a head shift from isocenter of +4 cm in the caudal direction.

DISCUSSION & CONCLUSIONS

> The lens dose reduction with the ROI attenuator is shown to vary with beam angulation and patient head position and between the left and right eyes.



Figure 2. (A) Head image acquired with an ROI attenuator with a circular hole and 20% transmission factor showing the periphery with reduced intensity due to reduced dose. (B) Mask image of the ROI attenuator derived by CNN from Figure 2A. (C) Final brightness corrected, and noise reduced image obtained from Figure 2A using the mask of Figure 2B⁵.

METHODS

- > The eye lens dose was calculated for the Zubal computational phantom⁶ using EGSnrc Monte-Carlo software as a function of gantry angulations from 0 to 90 degrees left anterior oblique (LAO) as shown in Figure 3, and for head shifts from isocenter as shown in Figure 4.
- \succ The beam files were generated for 80 kVp beams with 1.8 mm aluminum added beam filtration and square field sizes of 5x5 cm (small FOV) and 10x10 cm (large FOV).⁷



Figure 3: Gantry rotation **Figure 4.** Shift of the center of the head relative to the angles from 0° to 90° beam isocenter as used for lens dose calculations: LAO⁷ head shifts in (A) lateral X direction and (B) longitudinal Y direction. \succ For this study, the ROI projection was simulated as the combination of the large square 10 x 10 cm FOV and the small square 5 x 5 cm FOV representing the ROI as shown in Fig. 5.



Figure 7: (A) Axial cross section showing head shift in the -x direction and ROI attenuated beam for lateral and PA projections. (B) % LDR for right (R) and left (L) lens as a function of LAO gantry angle for different transmission factors for a head shift from isocenter of -4 cm in the lateral direction.



- \succ The least dose reduction occurs for angles when the eye lens is in the ROI, so the effect of the attenuator is on scatter dose.
- > Due to about 1 cm lateral tilt of Zubal head phantom,⁶ the right and left eyes are asymmetric relative to the head centerline, hence there is unequal dose reduction for the left and right lenses at 0 degrees LAO when the lateral shift is zero, as shown in Fig. 6.
- \succ With a head shift of -4 cm and +4 cm in the x direction (lateral), the lens dose reduction varies with gantry LAO angle and, for a 20% transmission factor, increases up to about 75% at higher LAO angles compared to a 10 x 10 cm FOV for both lenses (Figs. 7 and 8).
- \succ With a head shift of -4 cm and +4 cm along the y direction (longitudinal) there is a lens dose reduction of about 70% at LAO angles above 40 degrees for a 20% transmission factor with the ROI attenuator compared to a 10 x 10 cm FOV for both eye lens as shown in Figs. 9 and 10. Due to the lateral tilt of the Zubal head,⁶ the % LDR is not the same for the left and right lenses even with a 0 cm lateral shift.

 \succ The use of ROI attenuators allows visualization of full field information while providing a substantial reduction of lens dose, thereby reducing the risk of cataractogenesis during neuro-interventional procedures.

> The lens dose for a given projection with the ROI attenuator was then calculated as the weighted sum of the small-FOV lens dose (LD_{S}) and the large-FOV lens dose (LD_{I}) .

Figure 8: (A) Axial cross section showing head shift in the +x direction and ROI attenuated beam for lateral and PA projections. (B) % LDR for right (R) and left (L) lens as a function of LAO gantry angle for different transmission factors for a head shift from isocenter of +4 cm in the lateral direction.

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