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Bagga et al.

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- (54) **PLIABLE CONFORMABLE BONE RESTORATIVE**
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- (*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 227 days.

This patent is subject to a terminal disclaimer.

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(21) Appl. No.: **10/973,972**

(22) Filed: **Oct. 26, 2004**

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Related U.S. Application Data
(63) Continuation-in-part of application No. 10/771,077, filed on Feb. 3, 2004, now Pat. No. 7,189,263.

(51) **Int. Cl.**
A61F 2/28 (2006.01)

(52) **U.S. Cl.** **623/23.51**; 623/13.11; 623/23.53; 623/23.61; 424/422; 424/484; 514/2; 514/801

(58) **Field of Classification Search** None
See application file for complete search history.

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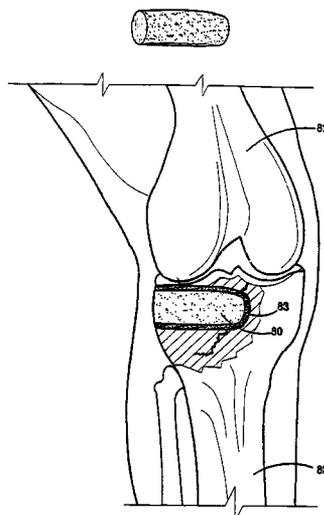
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(57) **ABSTRACT**

A pliable bone restorative having an osteoconductive foam that at least partially surrounds a biocompatible mesh and the foam comprises a biocompatible, resorbable polymer and calcium phosphate.

48 Claims, 26 Drawing Sheets



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FIG. 1A

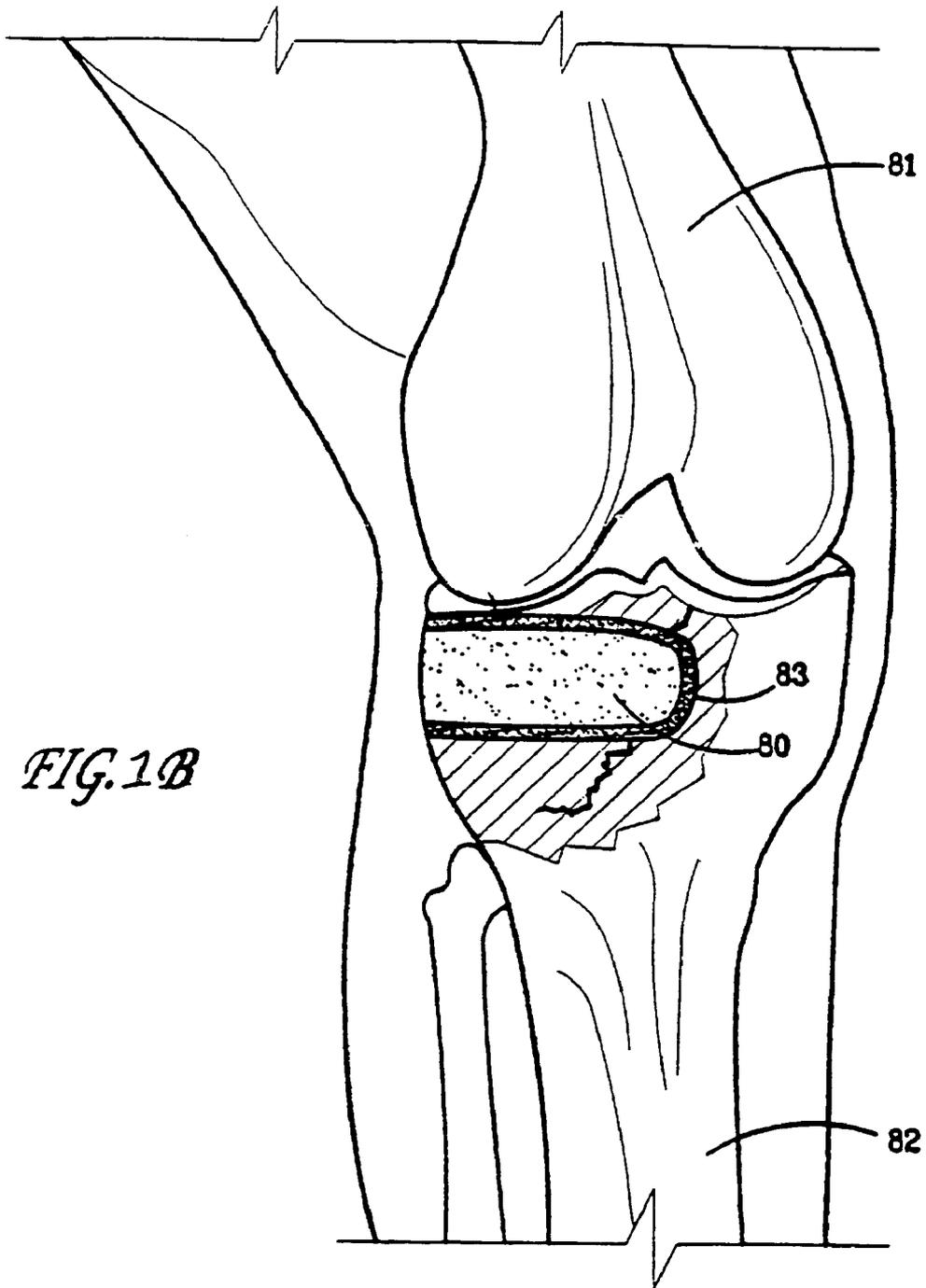


FIG. 1B

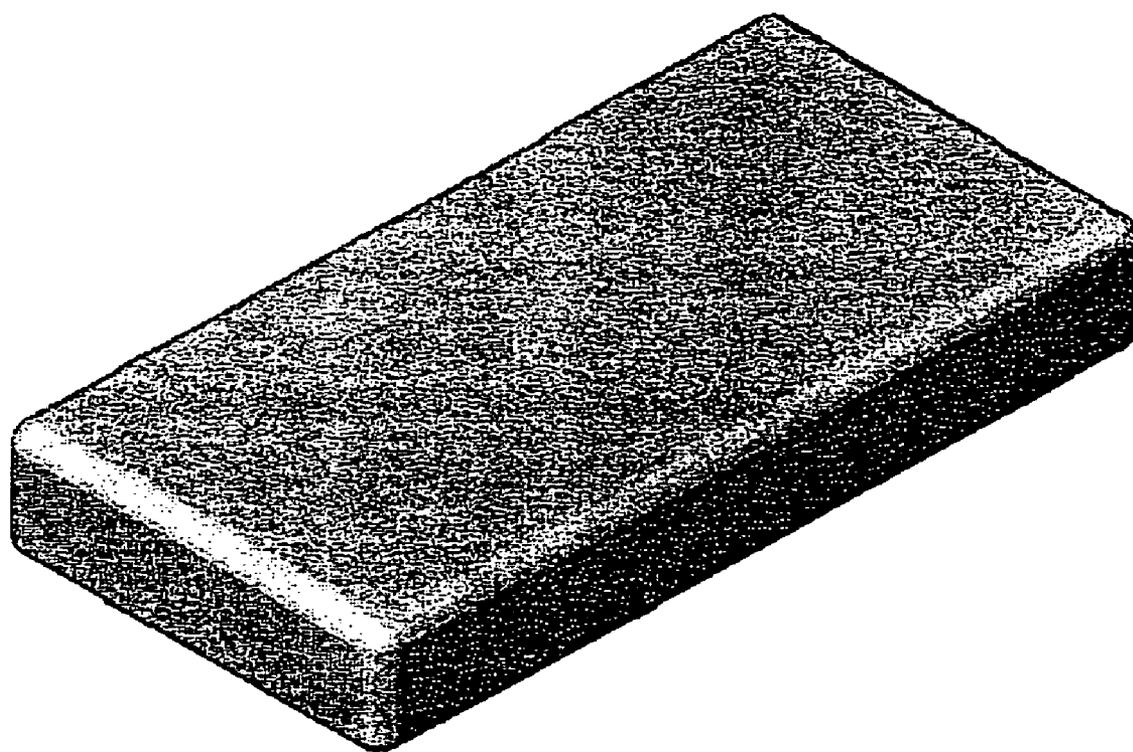


FIGURE 2

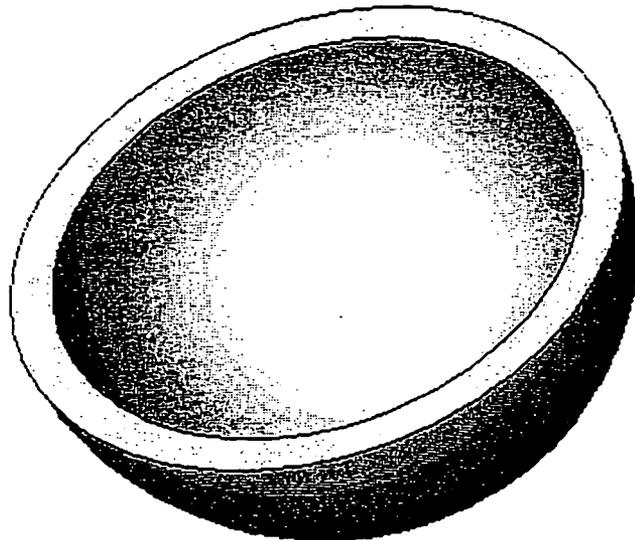
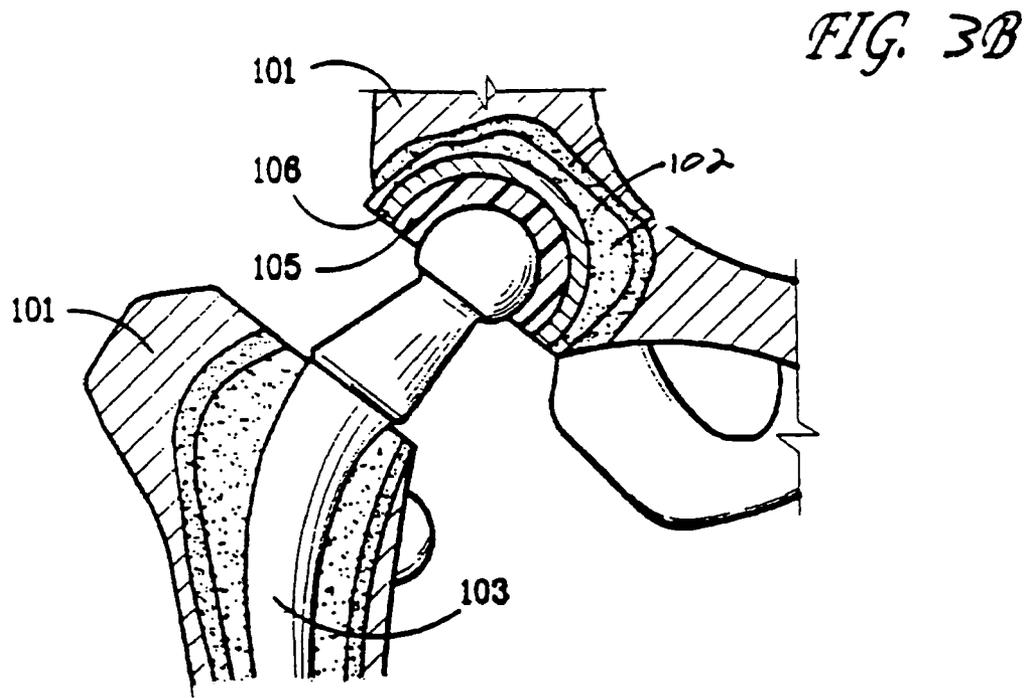


FIGURE 3A

FIG. 4B

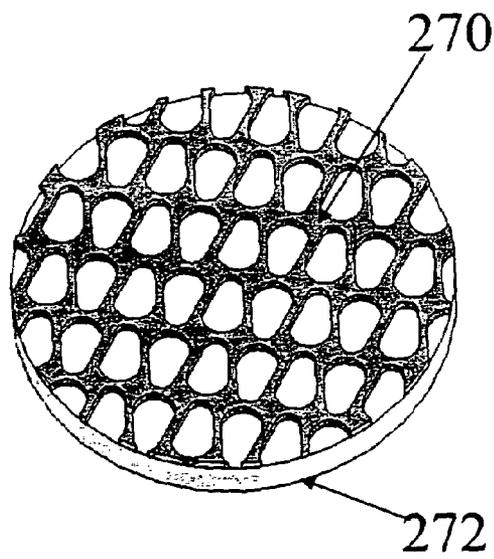
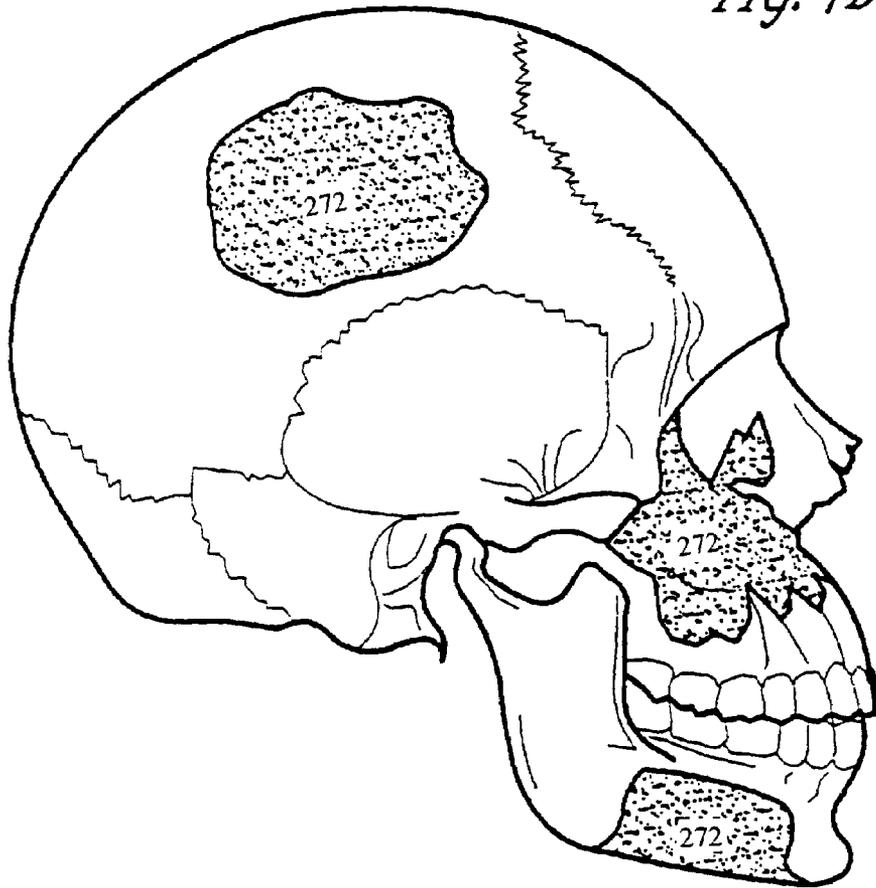


FIGURE 4A

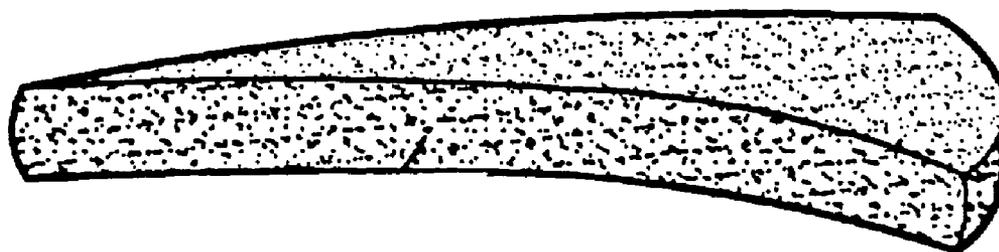


FIG. 5

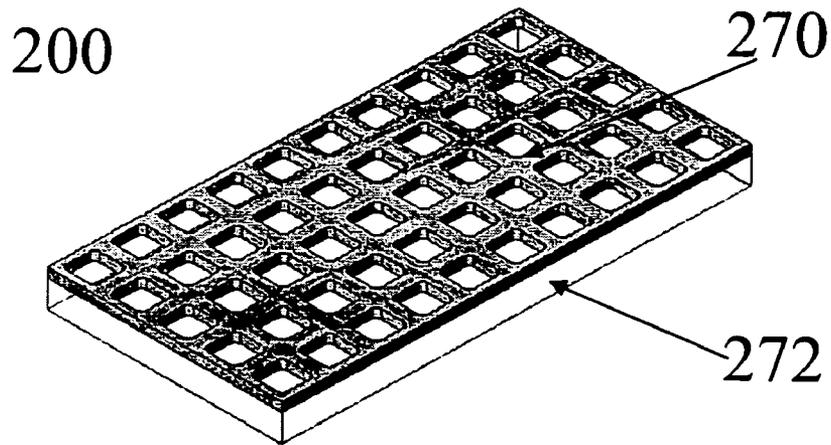


FIGURE 6A

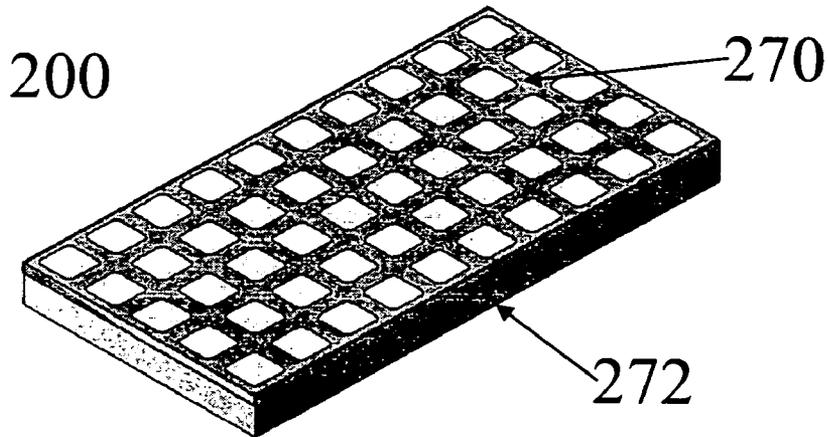


FIGURE 6B

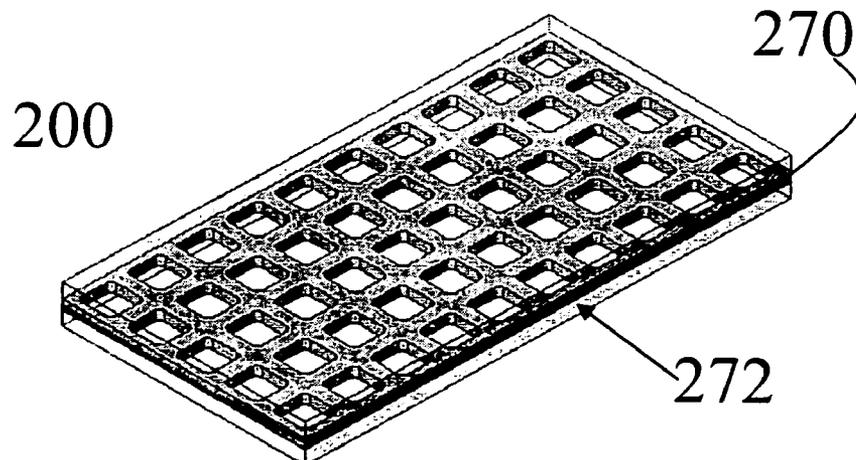


FIGURE 6C

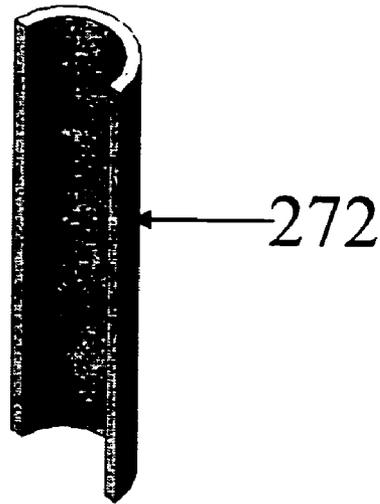


FIGURE 7A

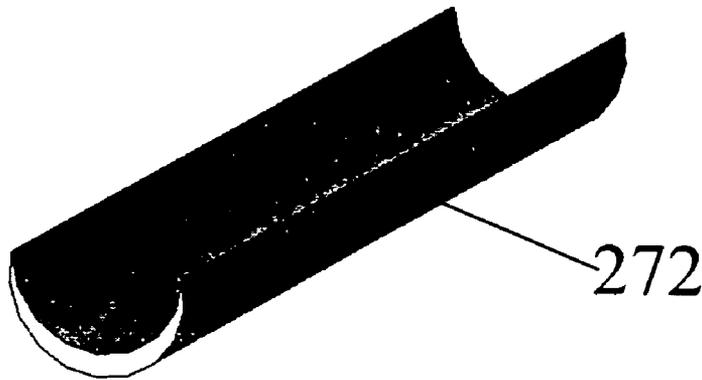


FIGURE 7B

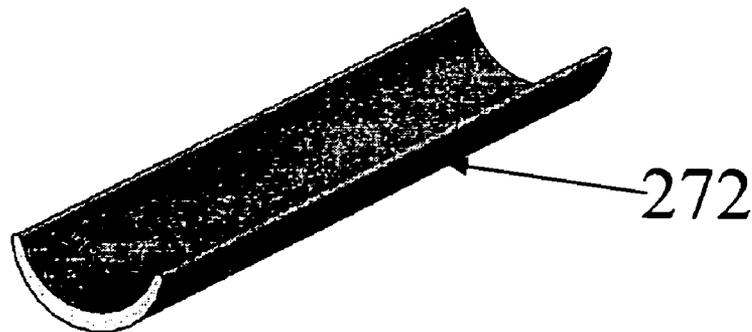


FIGURE 7C

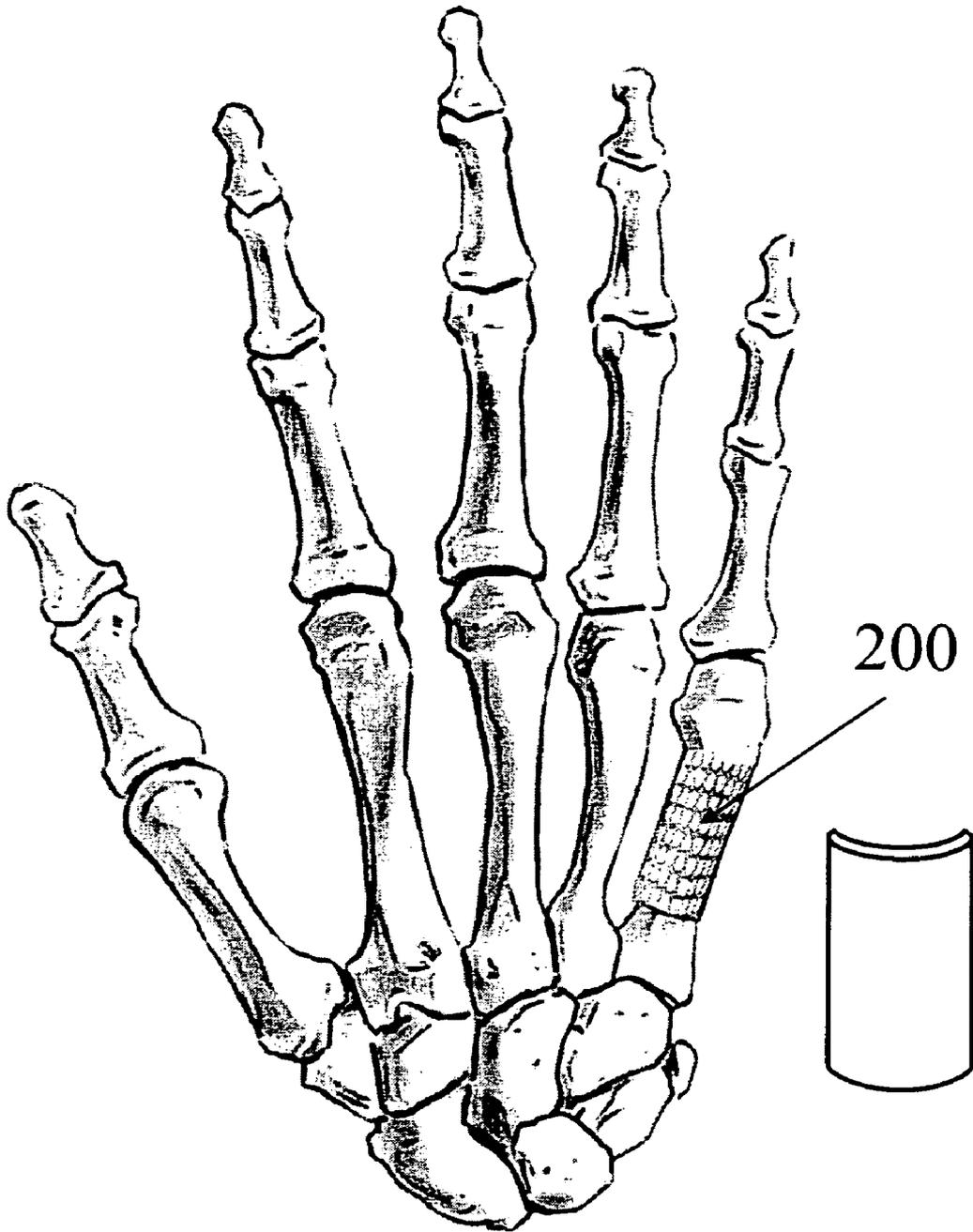


FIGURE 8

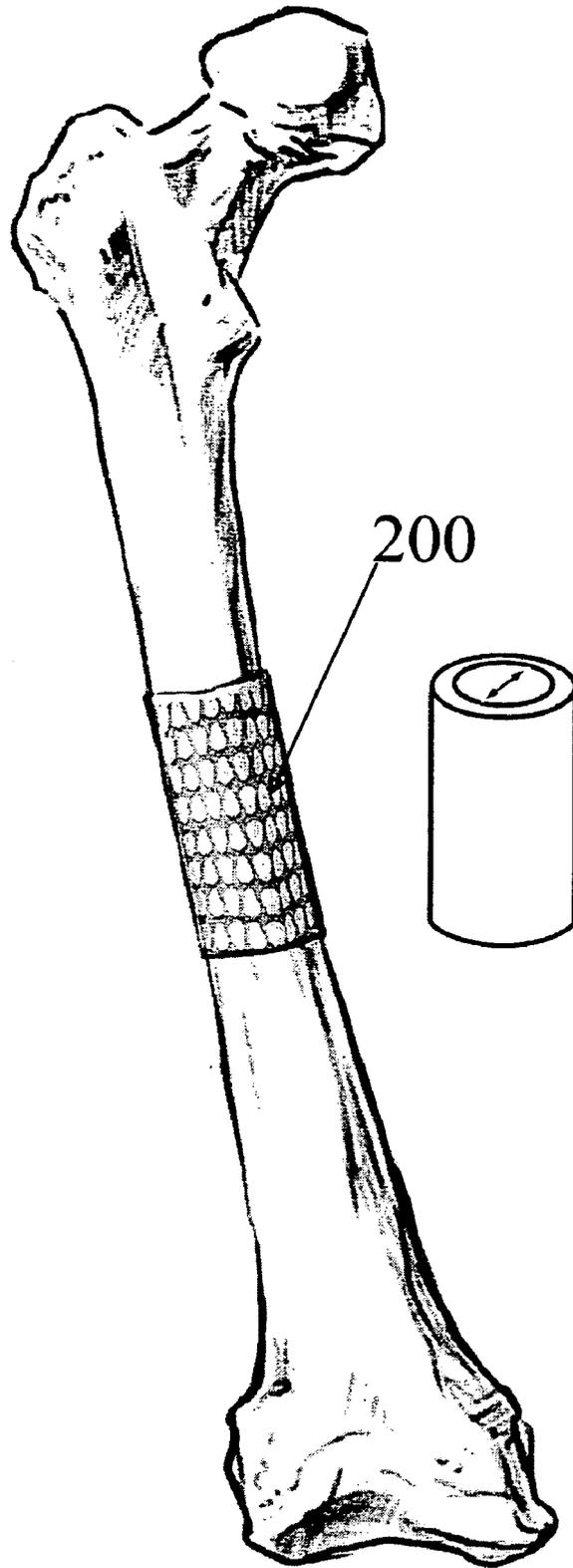


FIGURE 9

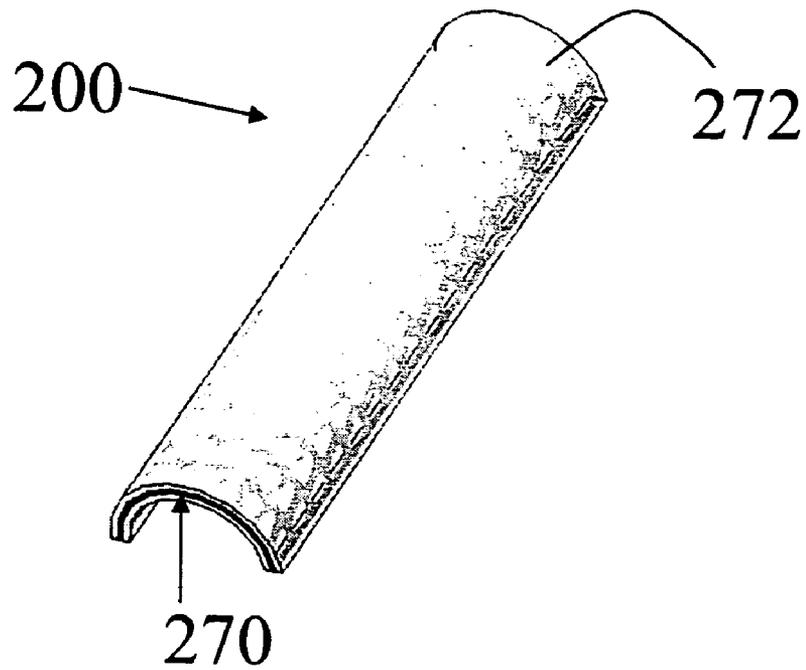


FIGURE 10A

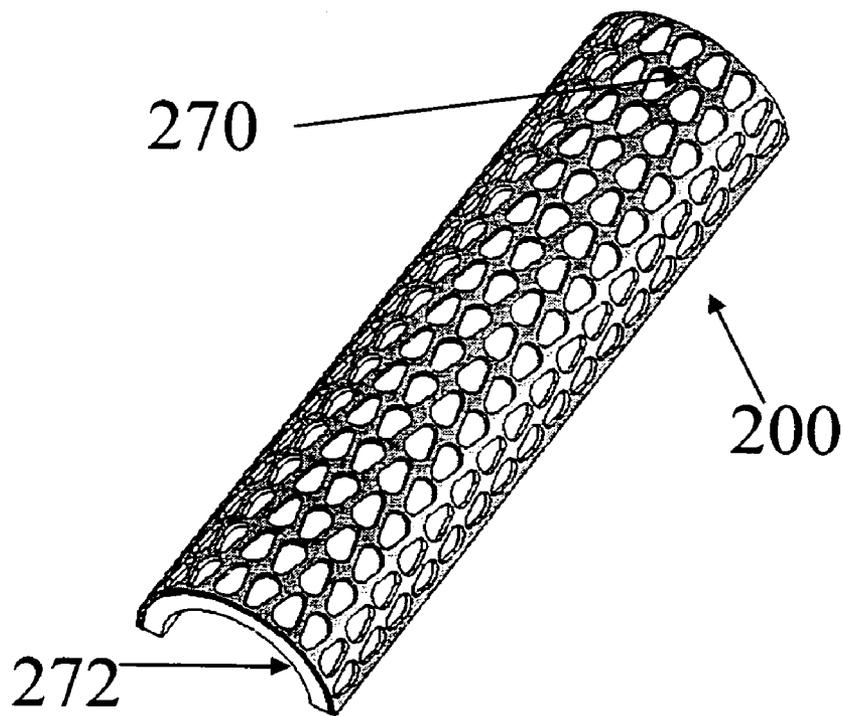


FIGURE 10B

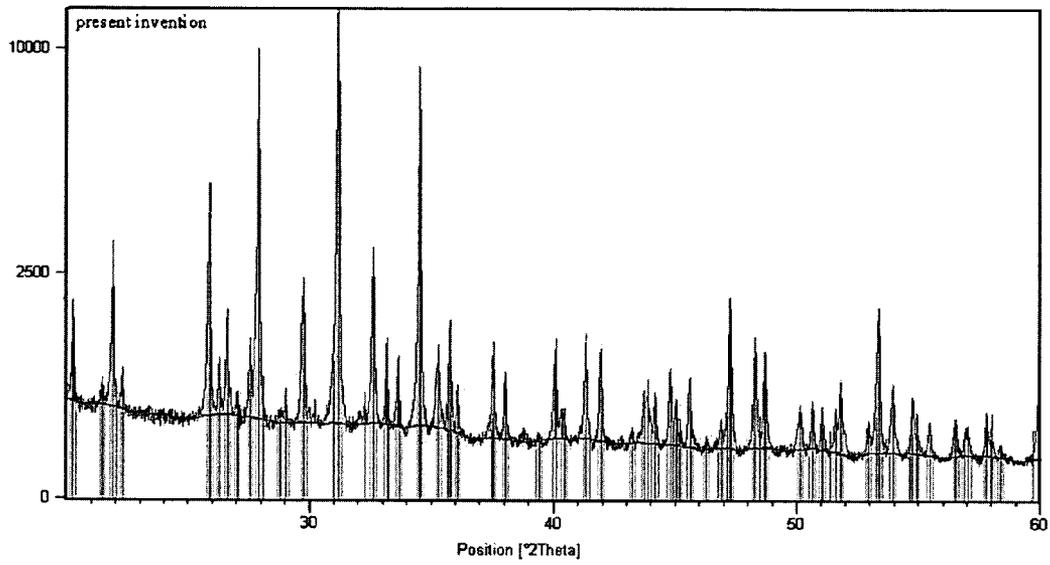


FIGURE 11

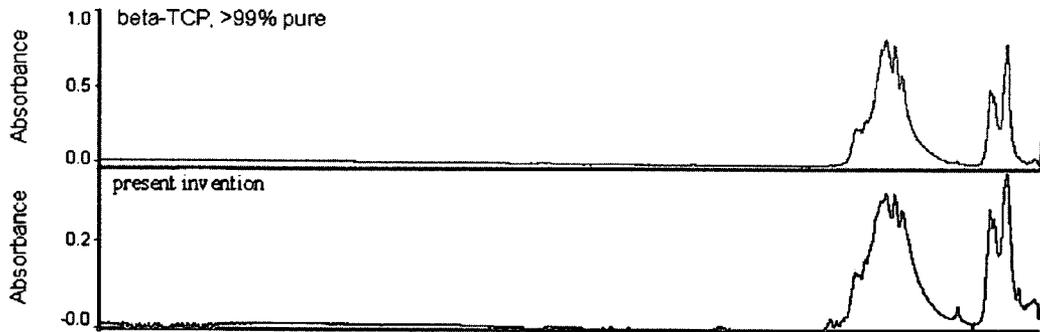


FIGURE 12

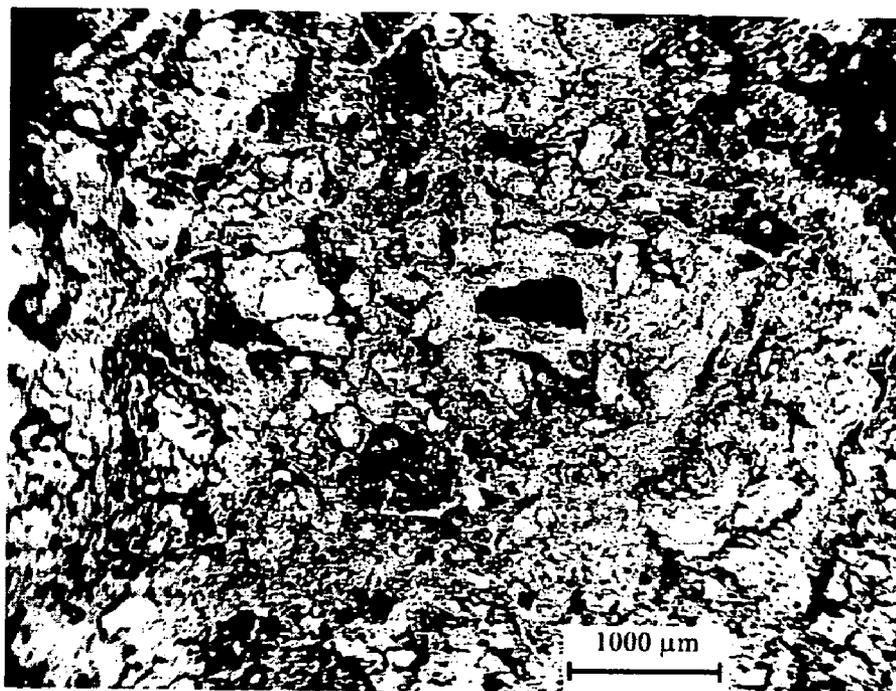


Figure 13

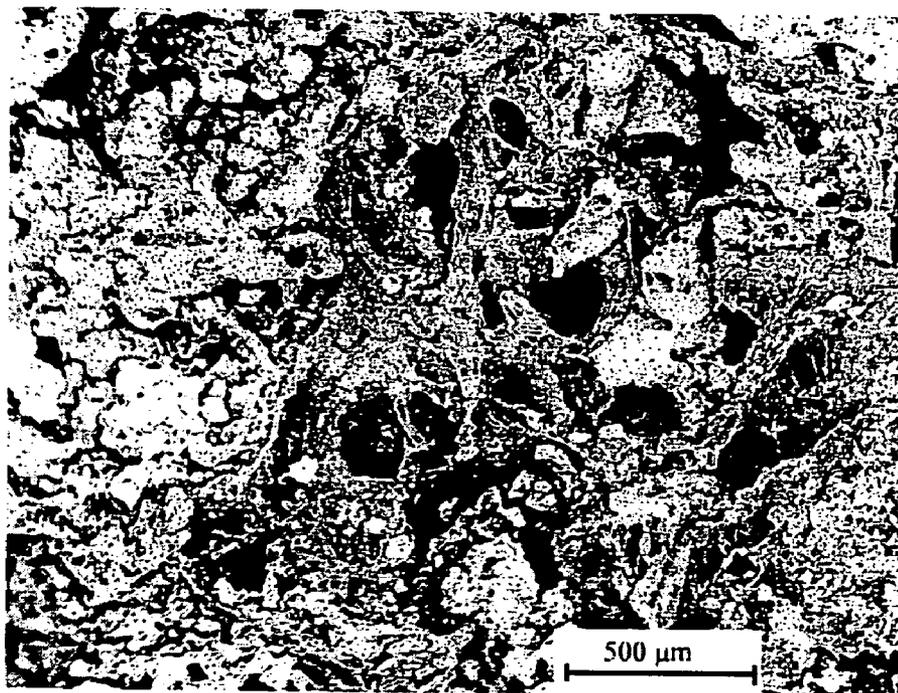


Figure 14

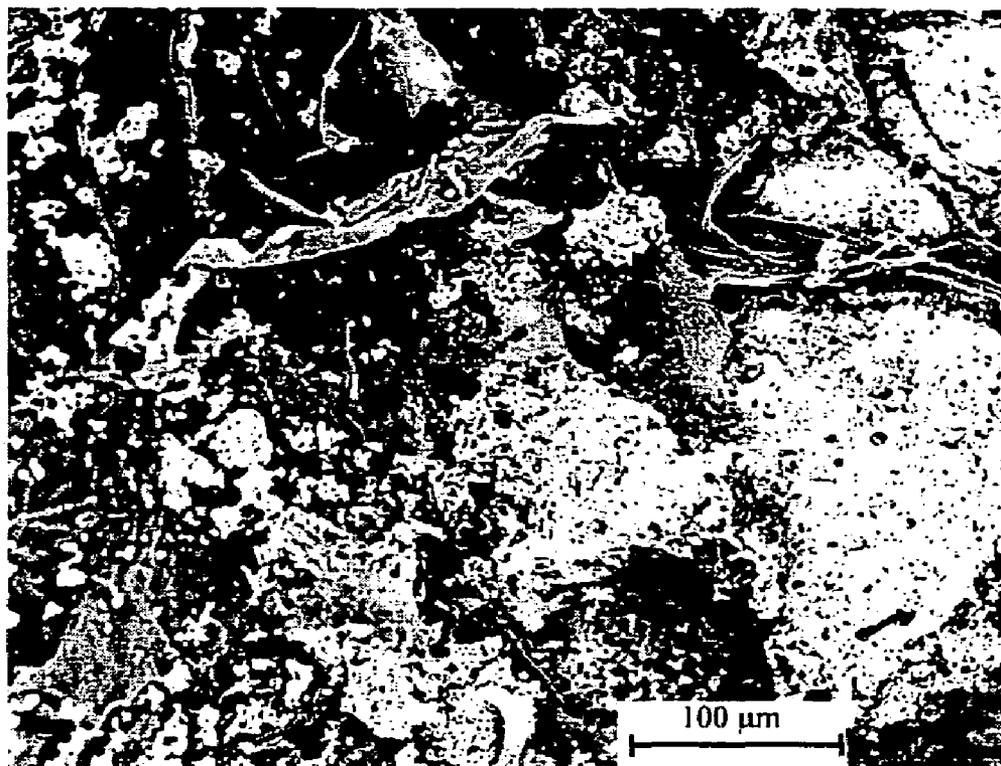


Figure 15

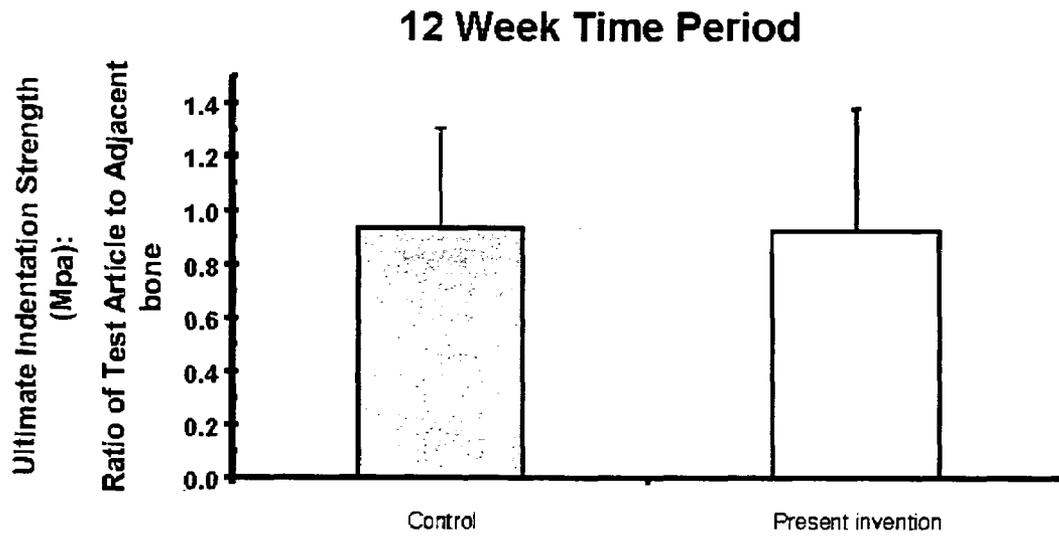


FIGURE 16

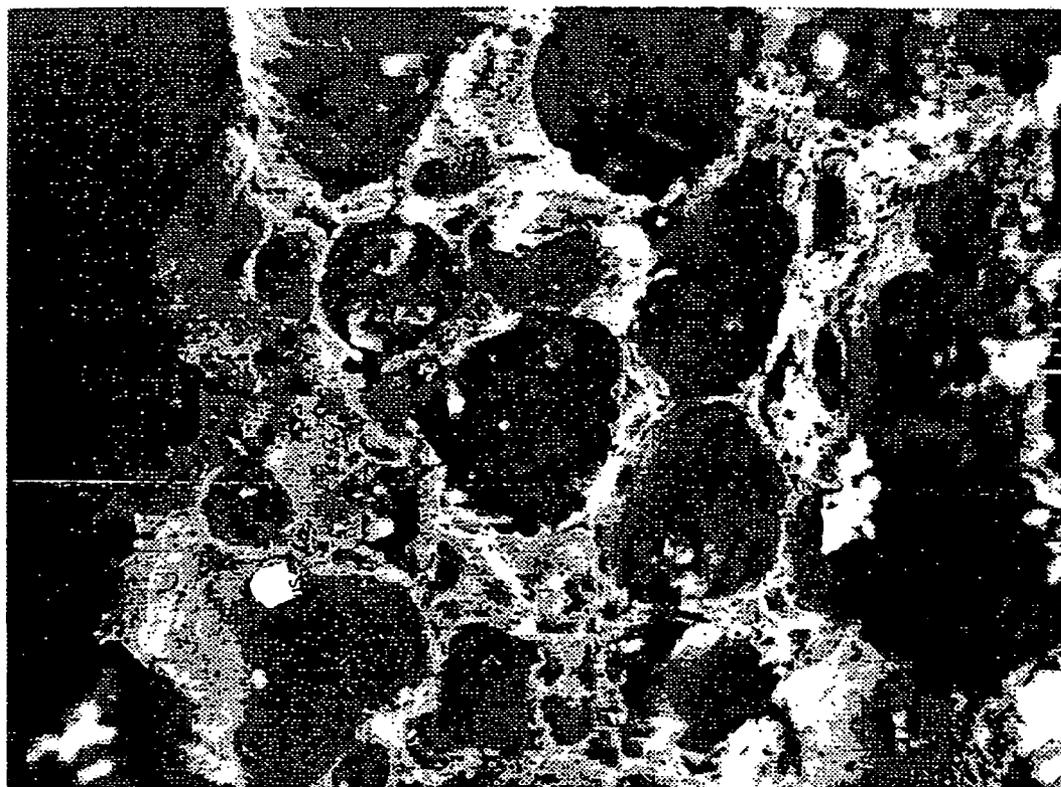


Figure 17

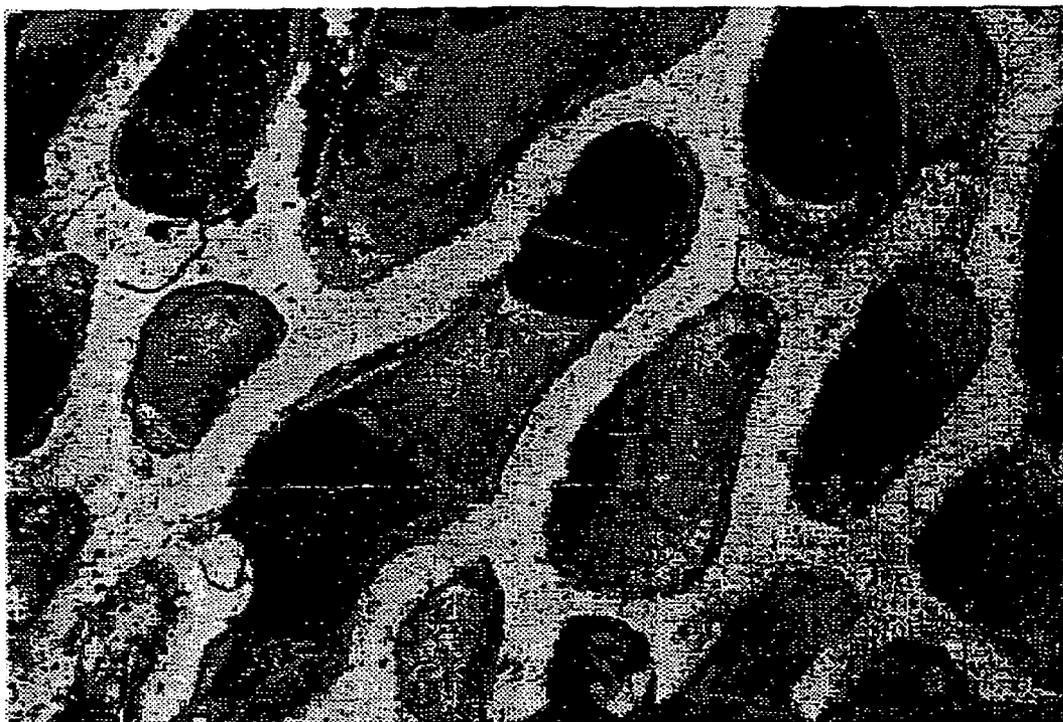


Figure 18

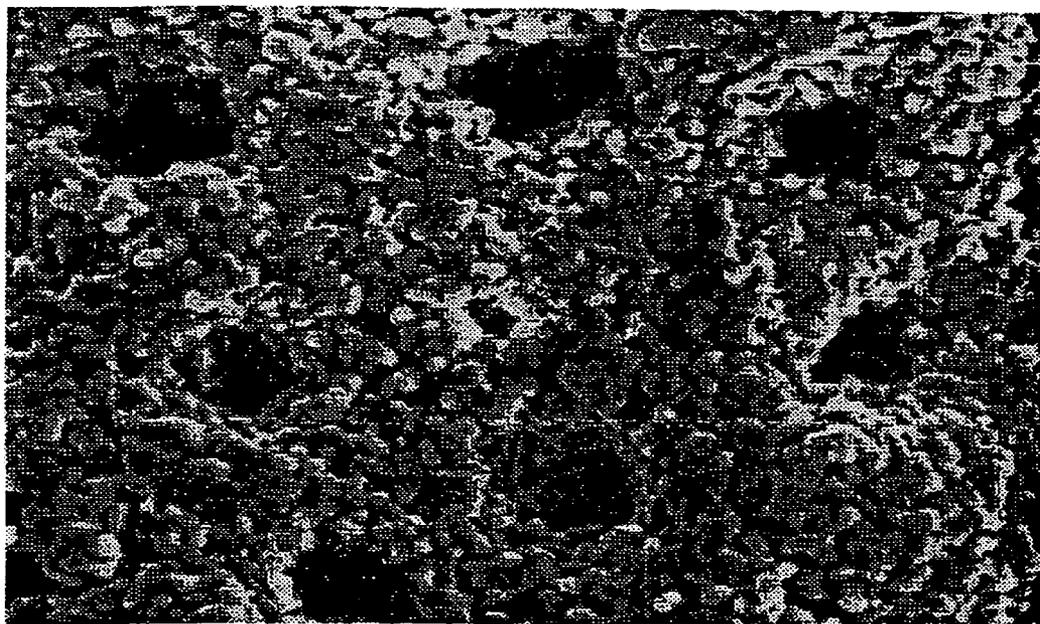


Figure 19

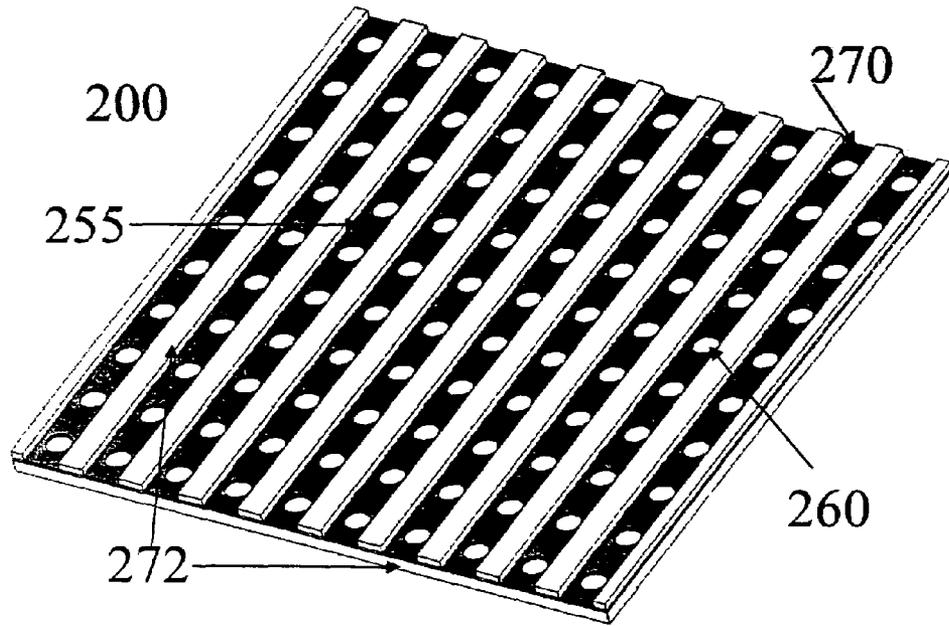


FIGURE 20A

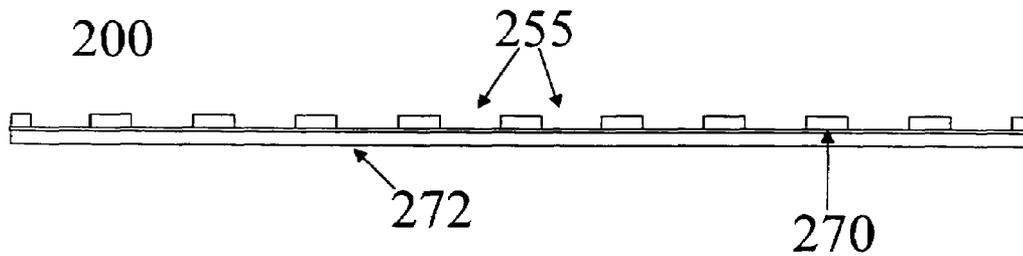


FIGURE 20B

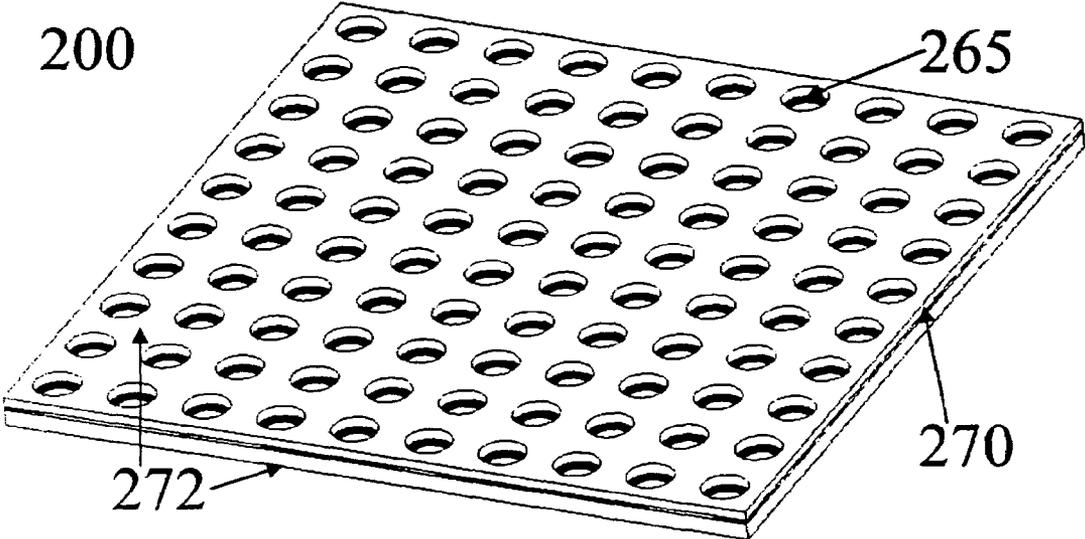


FIGURE 21

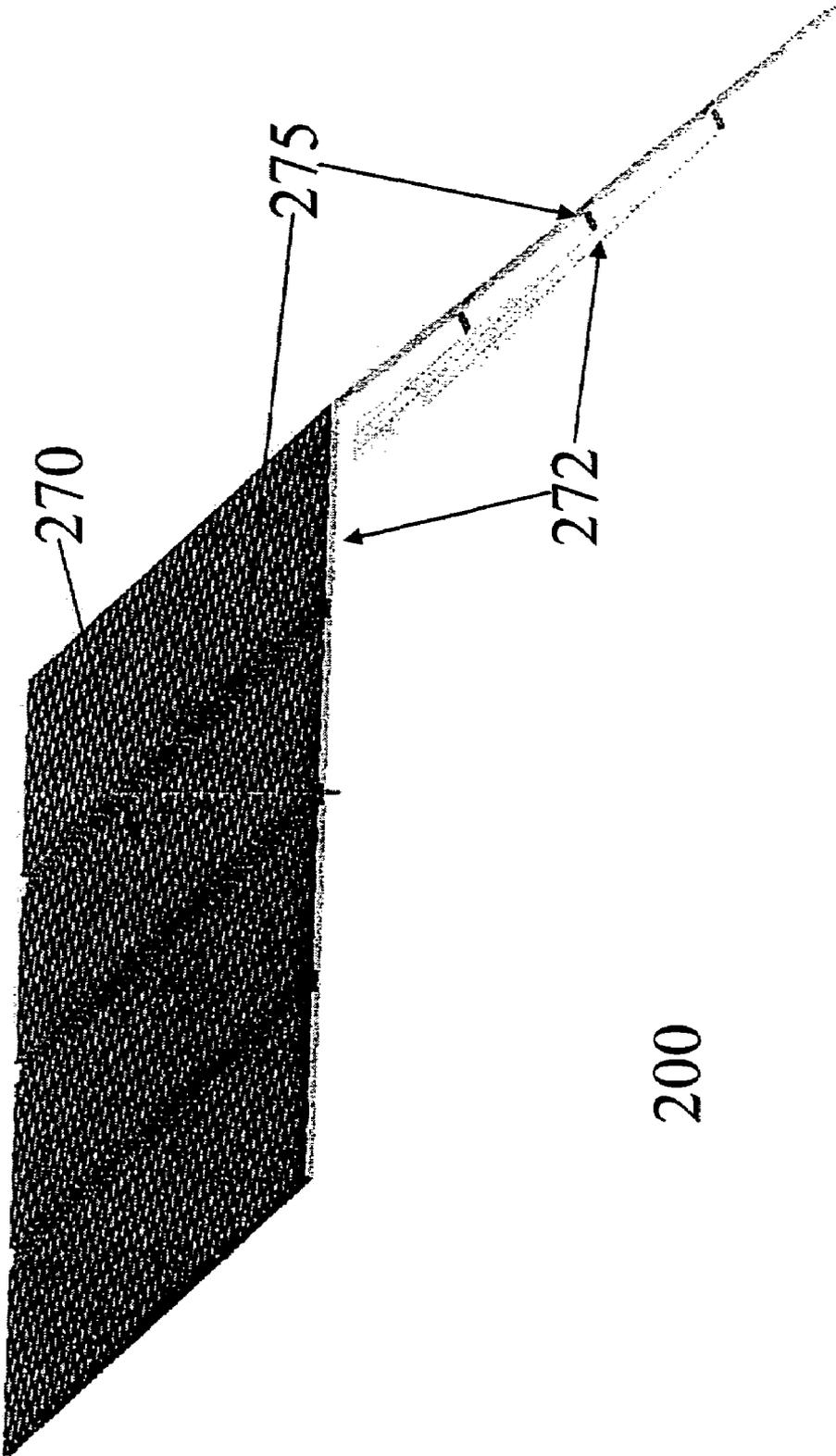


FIGURE 22

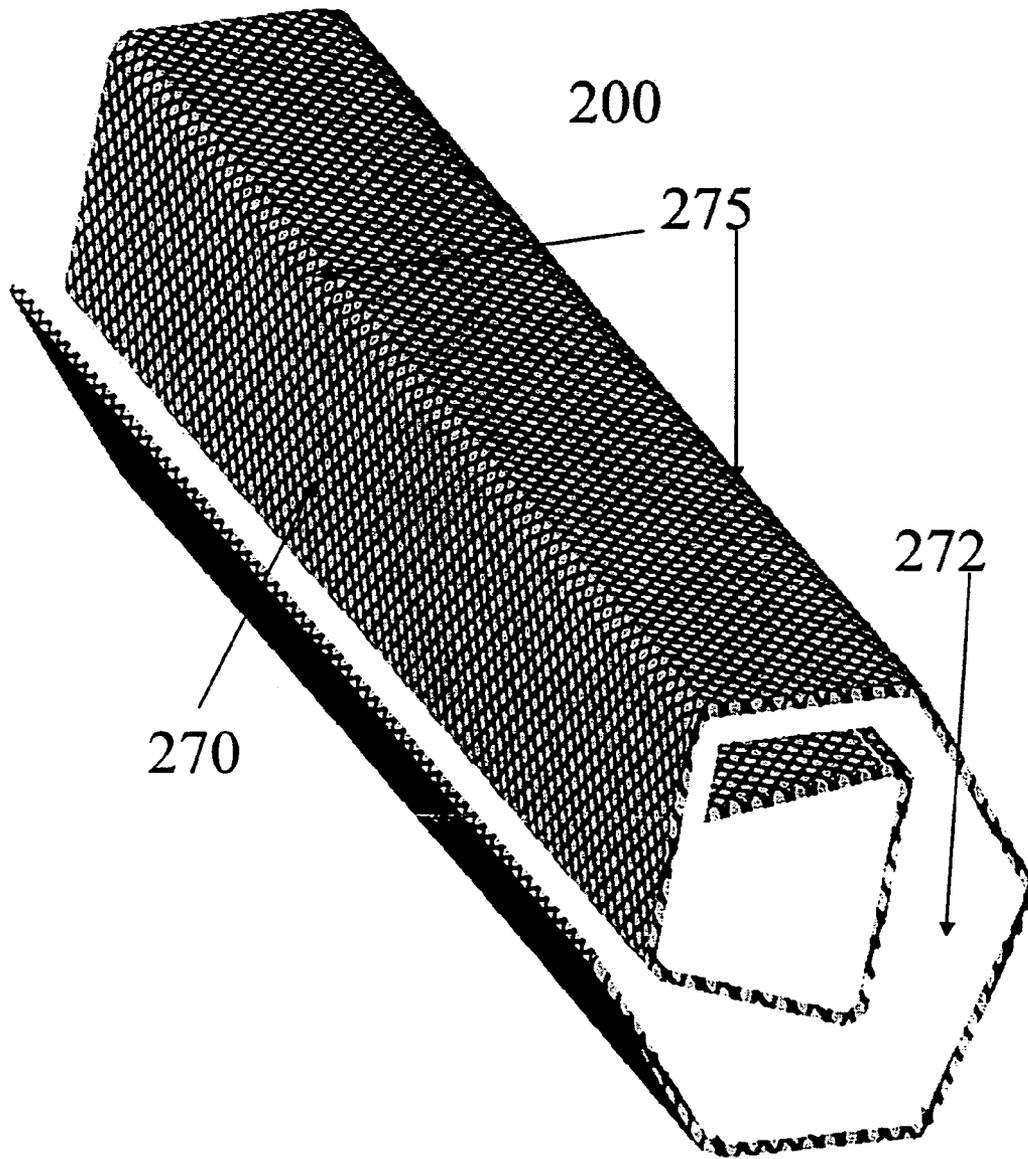


FIGURE 23

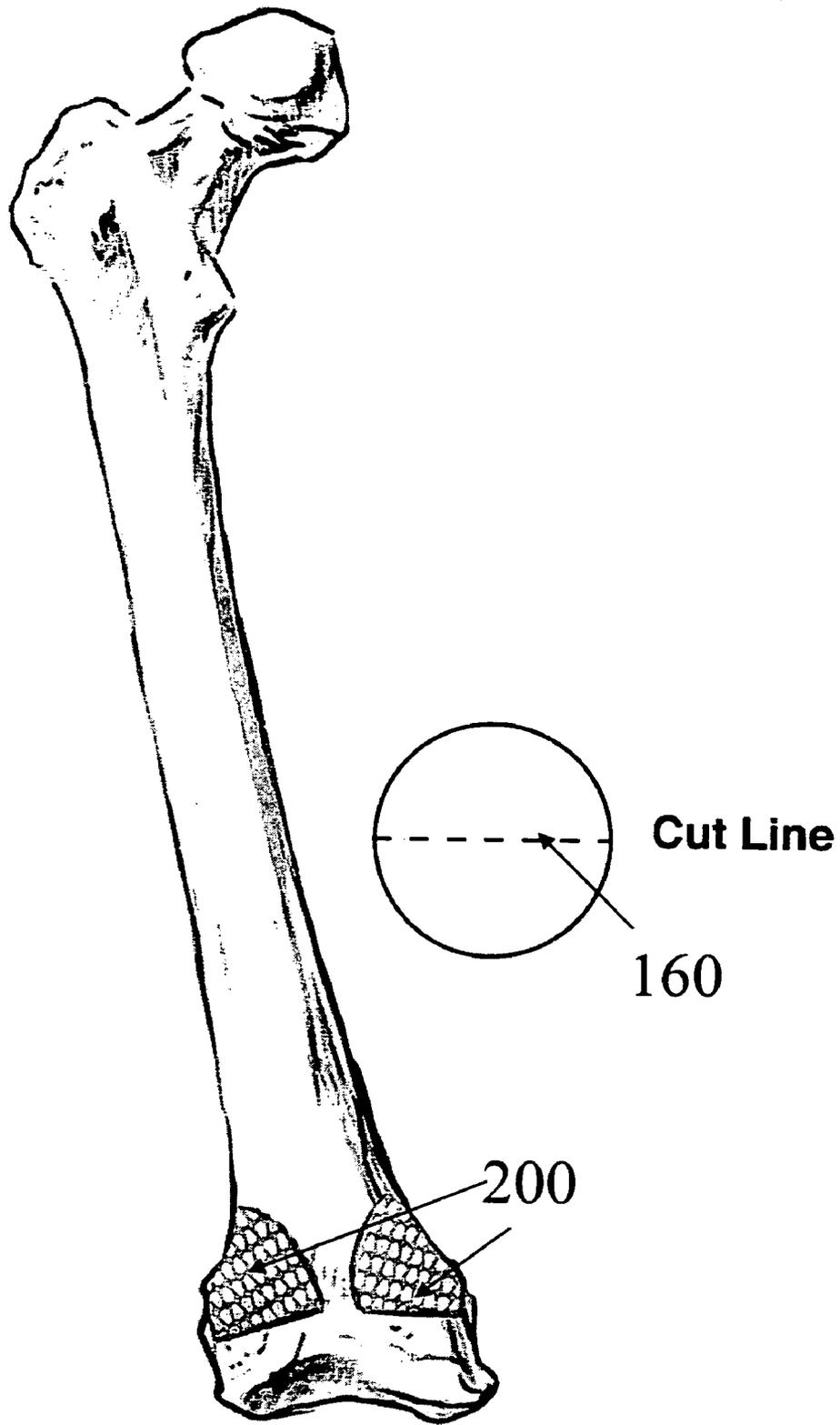


FIGURE 24

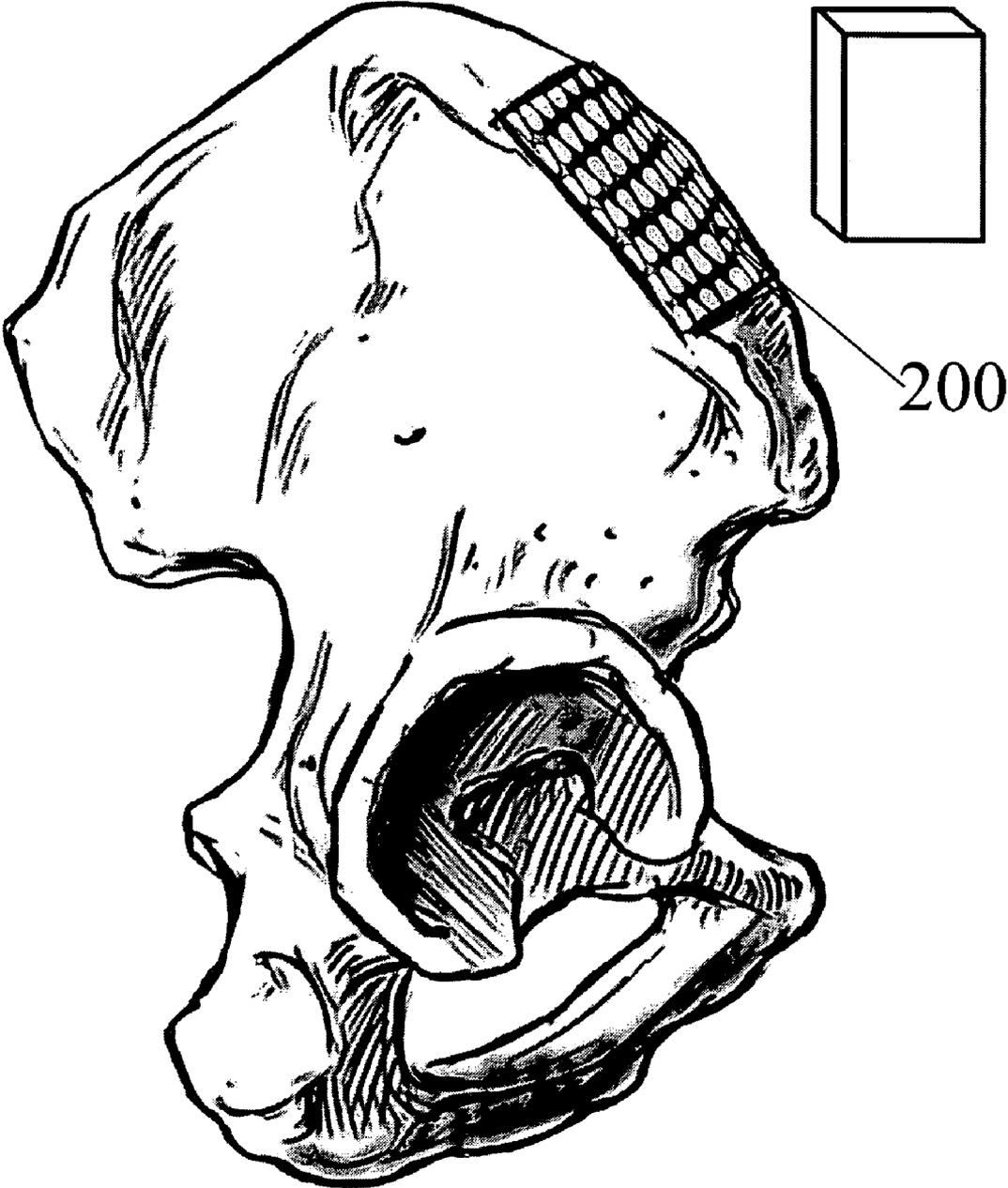


FIGURE 25

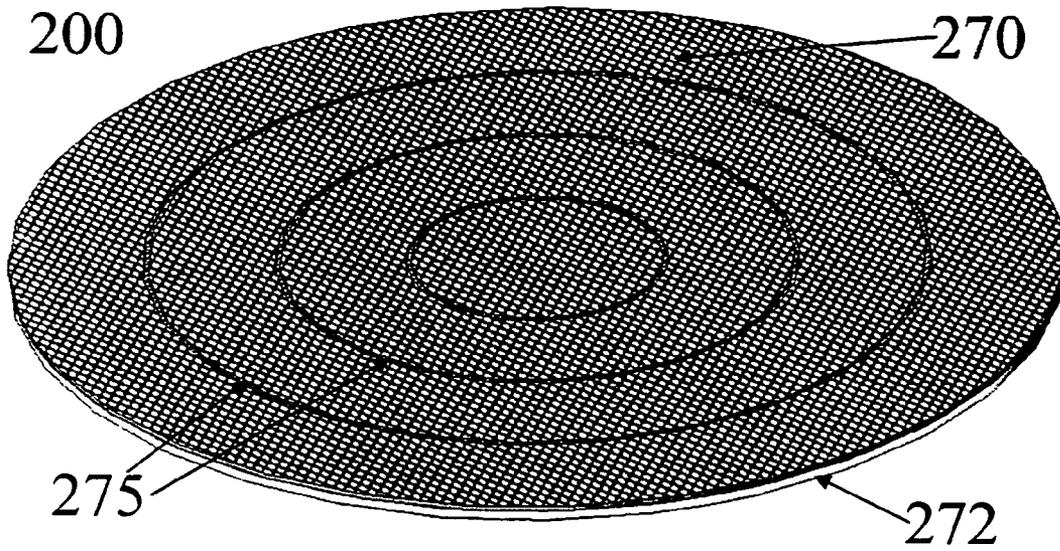


FIGURE 26A

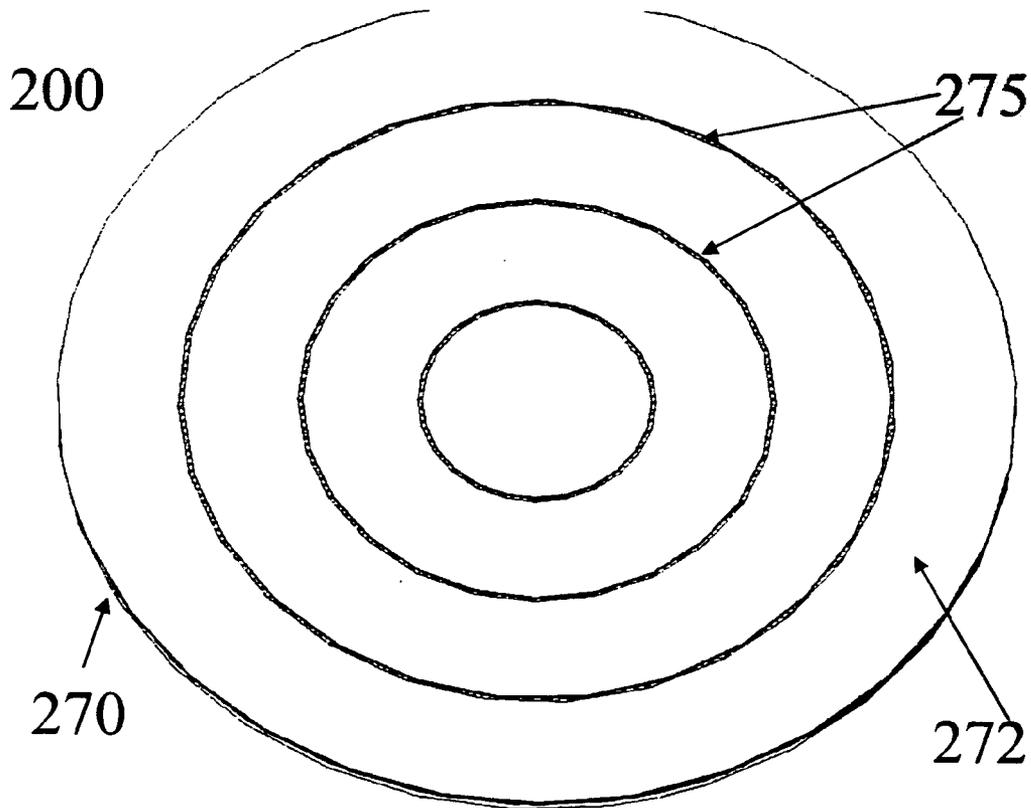


FIGURE 26B

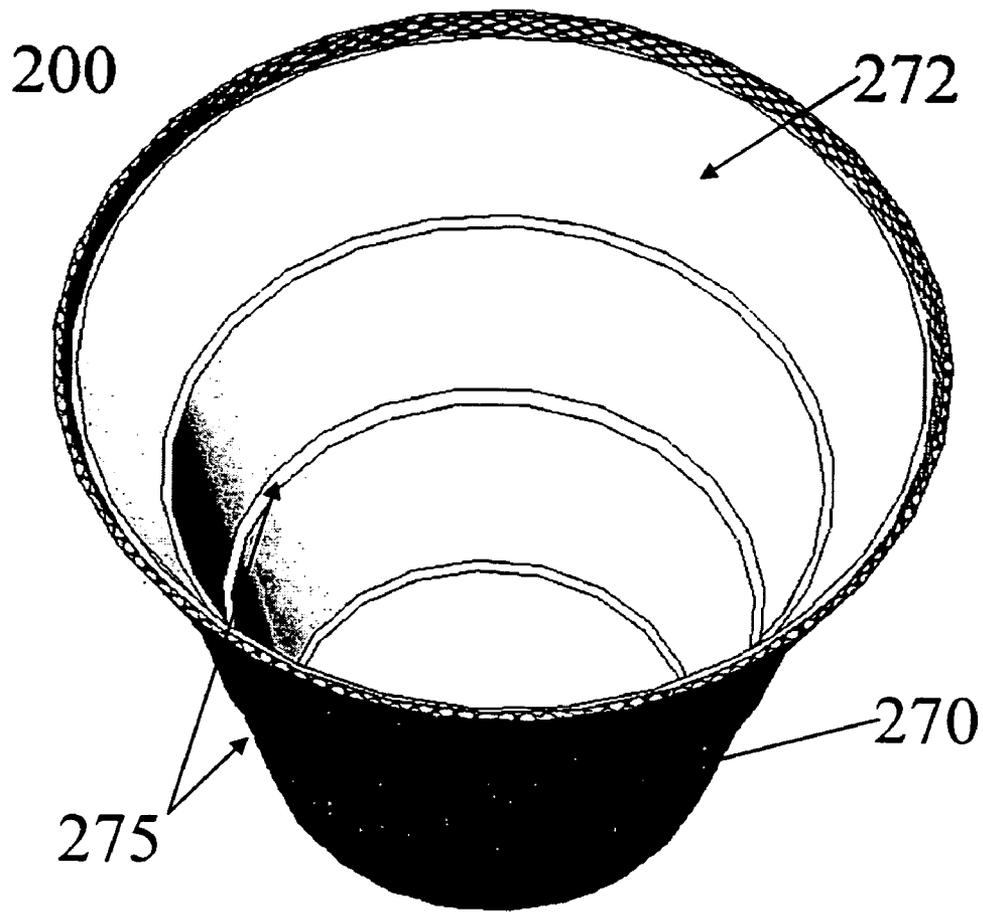


FIGURE 26C

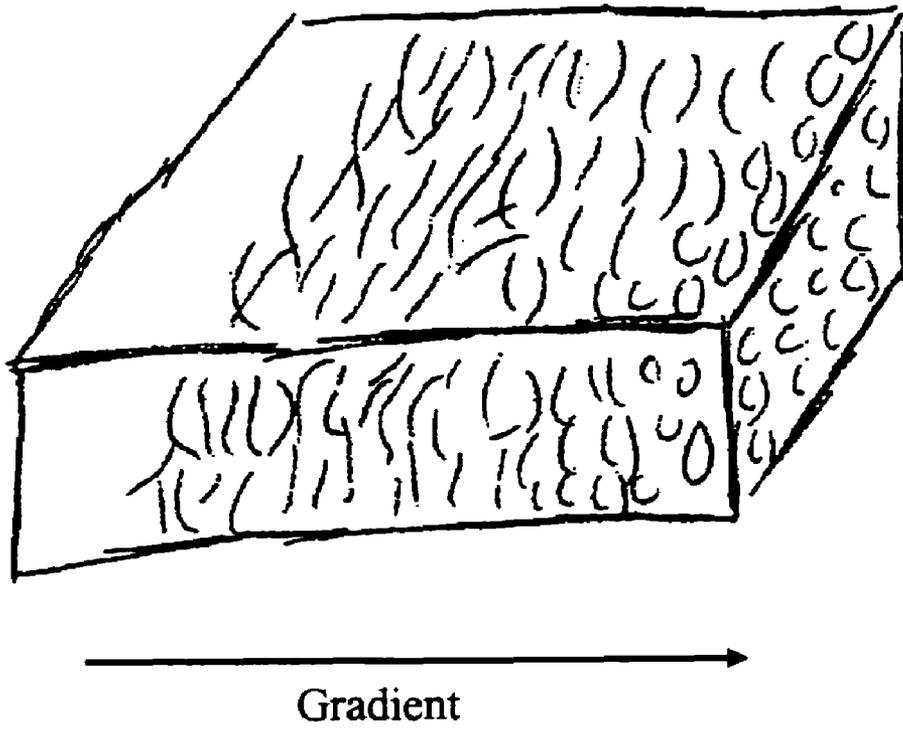


Figure 27

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**PLIABLE CONFORMABLE BONE
RESTORATIVE****CROSS-REFERENCE TO RELATED
APPLICATIONS**

This application is a Continuation-in-Part of U.S. application Ser. No. 10/771,077, which was filed Feb. 3, 2004, now U.S. Pat. No. 7,189,263, which is incorporated herein by reference in its entirety.

FIELD OF THE INVENTION

This invention relates to biocompatible bone graft materials for repairing bone defects and the application of the bone graft materials disclosed herein. The present invention incorporates the benefits of inorganic shaped bodies having macro, meso, and microporosity and polymers such as collagen.

BACKGROUND OF THE INVENTION

There has been a continuing need for improved bone graft materials. Although autograft, the current gold standard, may have very good properties and radiopacity, its use exposes patients to the risk of second surgeries, pain, and morbidity at the donor site. Allograft devices, which are processed from donor bone, also have very good radiopacity, but carry the risk of disease transmission. The devices are restricted in terms of variations on shape and size and have sub-optimal strength properties that decrease after implantation. The quality of the allograft devices varies because they are natural. Also, since companies that provide allograft implants obtain their supply from donor tissue banks, there tend to be limitations on supply. In recent years, synthetic materials have become a viable alternative to autograft and allograft devices. One such synthetic material is Vitoss® Scaffold Synthetic Cancellous Bone Void Filler (Orthovita, Inc., Malvern, Pa., assignee of the present application). Synthetic graft materials, like autograft and allograft, serve as osteoconductive scaffolds that promote the ingrowth of bone. As bone growth is promoted and increases, the graft material resorbs and is eventually replaced with new bone.

Many synthetic bone grafts include materials that closely mimic mammalian bone, such as compositions containing calcium phosphates. Exemplary calcium phosphate compositions contain type-B carbonated hydroxyapatite $[Ca_5(PO_4)_3x(CO_3)_x(OH)]$, which is the principal mineral phase found in the mammalian body. The ultimate composition, crystal size, morphology, and structure of the body portions formed from the hydroxyapatite are determined by variations in the protein and organic content. Calcium phosphate ceramics have been fabricated and implanted in mammals in various forms including, but not limited to, shaped bodies and cements. Different stoichiometric compositions such as hydroxyapatite (HAp), tricalcium phosphate (TCP), tetracalcium phosphate (TTCP), and other calcium phosphate salts and minerals, have all been employed to match the adaptability, biocompatibility, structure, and strength of natural bone. The role of pore size and porosity in promoting revascularization, healing, and remodeling of bone has been recognized as a critical property for bone grafting materials. The preparation of exemplary porous calcium phosphate materials that closely resemble bone have been disclosed, for instance, in U.S. Pat. No. 6,383,519 (hereinafter the '519 patent") and U.S. Pat. No. 6,521,246 (hereinafter the '246 patent"), incorporated herein by reference in their entirety.

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There has been a continued need for improved bone graft systems. Although calcium phosphate bone graft materials are widely accepted, they lack the strength, handling and flexibility necessary to be used in a wide array of clinical applications. Heretofore, calcium phosphate bone graft substitutes have been used in predominantly non-load bearing applications as simple bone void fillers and the like. For more clinically challenging applications that require the graft material to take on load, bone reconstruction systems pair a bone graft material with traditional rigid fixation systems. The prior art discloses such bone reconstruction systems. For instance, MacroPore OS™ Reconstruction System is intended to reinforce and maintain the relative position of weak bony tissue such as bone graft substitutes or bone fragments from comminuted fractures. The system is a resorbable graft containment system composed of various sized porous sheets and sleeves, non-porous sheets and sleeves, and associated fixation screws and tacks made from polylactic acid (PLA). However, the sheets are limited in that they can only be shaped for the body when heated.

The Synthes SynMesh™ consists of flat, round, and oval shaped cylinders customized to fit the geometry of a patient's anatomical defect. The intended use is for reinforcement of weak bony tissue and is made of commercially pure titanium. Although this mesh may be load bearing, it is not made entirely of materials that are flexible.

There is a need for resorbable bone grafts with improved handling, which are flexible and not brittle, and are compression resistant. It has been discovered that admixing highly porous resorbable inorganic bodies with resorbable polymeric materials greatly improves upon handling, yet still provides an osteoconductive implant with good resorption and bone formation properties. It will be appreciated that such an implant would offer an easy-to-use dose of composite material and would be an advancement over current bone reconstruction systems for certain clinical applications in that it eliminates the need to have both a separate graft material and rigid fixation system.

There is a need in this field to provide biocompatible graft materials with exceptional osteoconductive properties; to provide pre-sized graft materials in a variety of forms, including strips and cylinders for restoring defects in bone; to provide bone graft materials that can be shaped; and to provide bone graft materials with improved handling properties, so that the graft material can be cut dry or after being wetted and does not crumble.

Currently, bone grafts often are incapable of retaining fluids once a surgeon attempts to implant the graft into a bony space. The fluids are flushed out of the graft when manipulated by the surgeon. There is also a need to provide bone graft materials with some compression resistance, such that the brittleness often associated with inorganic or ceramic bone graft materials is eliminated; to provide bone graft materials with integrity that are at least partially load bearing; to provide bone graft materials with improved pliability that still retain high degrees of porosity over a broad pore size distribution to maintain superior resorption and bone ingrowth properties; to provide bone graft materials with fluid wicking and retention properties even under compressive loads; and to provide bone grafts that provide easy implantation into a bony space and with decreased tendency to wash away when imbued with fluid.

Additional advantages, and novel features of this invention will become apparent to those skilled in the art upon examination of the following descriptions, figures and claims thereof, which are not intended to be limiting.

SUMMARY OF THE INVENTION

The present invention is directed to pliable bone restorative comprising an osteoconductive foam comprising biocompatible, resorbable polymer and calcium phosphate that at least partially surrounds a biocompatible mesh.

Other embodiments of the present invention include pliable bone restoratives comprising a biocompatible mesh and at least partially surrounding the mesh, a biocompatible, resorbable polymer, and the oxidation-reduction reaction product of at least one metal cation, at least one oxidizing agent, and at least one oxidizable precursor anion. Disclosed herein are also pliable bone restoratives comprising a biocompatible mesh and a bone graft material comprising biocompatible, resorbable collagen and calcium phosphate. A further embodiment of the present invention is a pliable bone restorative comprising a biocompatible mesh and a biocompatible bone graft material comprising biocompatible, resorbable collagen and calcium phosphate having macro, meso, and microporosity. Also disclosed within are pliable bone restoratives comprising a biocompatible, resorbable substantially homogenous blend of a first polymeric material and a second material having interconnected macro, meso-, and microporosity, with said blend at least partially surrounding a biocompatible mesh. A further embodiment that may be preferred is in the form of a shaped body selected to conform generally to a mammalian, anatomical tissue structure. The shaped body comprises a polymer and beta tricalcium phosphate partially surrounding a biocompatible mesh. The graft may have interconnected macro-, meso-, and microporosity.

In some embodiments that may be preferred the selected polymer is collagen. The restorative may also be wetted with a fluid comprising bone marrow aspirate, cell concentrate, liquid hemostat, fibrin sealant, blood, or saline in some embodiments. The restorative may also be made in a variety of shapes including but not limited to cylindrical, block, cup, sleeve, or discoid shape.

A variety of materials may be selected to form the mesh portion of the restorative depending on the embodiment selected. The mesh may comprise titanium, stainless steel, nitinol, a polymer, a composite polymer, or some other composite blend. Titanium may be used in those embodiments specifically preferred. Similar to the bone graft material, the mesh may also exhibit varying degrees of porosity. In some embodiments, the mesh may have a predetermined porosity and thickness. The mesh may exhibit a number of surface textures and chemical treatments adequate for use in the body. The mesh may also be completely surrounded by the foam of the bone restorative.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1A illustrates one basic form of the biocompatible graft material in cylinder form. FIG. 1B depicts the graft material in cylindrical form **80** inserted into a bone void **83** below the femur **81** in the tibial plateau **82** within a human knee.

FIG. 2 illustrates another basic form of the present invention in strip form.

FIG. 3A illustrates one embodiment of the biocompatible graft material of the present invention in semi-spherical form used as a graft containment device. FIG. 3B depicts a semi-spherical form of the graft material **102** used to accommodate an artificial implant **103**. The graft material **102** contains an acetabular cup **106**, which holds a polyethylene cup **105**, in this embodiment.

FIG. 4A illustrates the bone restorative of the present invention in disc form. FIG. 4B illustrates another embodiment of the biocompatible graft material of the present invention used as a cranio-maxillofacial **76**, zygomatic reconstruction **72**, and mandibular implant **74**.

FIG. 5 illustrates one embodiment of a bone graft material described shaped into a block/wedge form and used as a tibial plateau reconstruction that is screwed, bonded, cemented, pinned, anchored, or otherwise attached in place.

FIGS. 6A and 6B illustrate synthetic resorbable defect filling bone graft materials **272** for bone restoration having mesh **270** attached to one side. FIG. 6C depicts a synthetic resorbable defect filling bone graft material block in which the mesh **270** is placed between the graft material **272**.

FIGS. 7A, 7B, and 7C illustrate the shapes of some embodiments in semi-tubular form used as a long bone reinforcement sleeve. As shown in the figures, the semi-tube may have a moon cross-section with a uniform thickness (FIG. 7A); or a crescent moon cross-section with a tapered radius that comes to a point (FIG. 7B) or a tapered radius that is rounded on the edges (FIG. 7C).

FIG. 8 depicts the semi-tubular shaped embodiment **200** placed on a metacarpal bone.

FIG. 9 depicts a tubular shaped embodiment **200** fitted around the femur.

FIGS. 10A and 10B depicts semi-tubular embodiments **200** showing different configurations for placing the biocompatible mesh **270** and graft material **272**.

FIG. 11 is a representative XRD spectra of a bone graft material of the present invention (top) vs. β -TCP (bottom).

FIG. 12 is a representative FTIR spectrum of bone graft material of the present invention vs. β -TCP (beta-TCP) and Predicate.

FIG. 13 is an SEM of the bone graft material, 20 \times .

FIG. 14 is an SEM of the bone graft material, 50 \times .

FIG. 15 is an SEM of the bone graft material, 250 \times .

FIG. 16 depicts the Ultimate Indentation Strength for one embodiment of the bone graft material vs. control normalized by adjacent bone at 12 weeks.

FIG. 17 is an SEM of air-dried gelatin treated inorganic material, 23 \times .

FIG. 18 is an SEM of sheep trabecular bone, 25 \times .

FIG. 19 is an SEM of the material shown in FIG. 14, 2000 \times .

FIG. 20A depicts an embodiment of the bone restorative **200** having channels **255** in the foam **272** so that a surgeon can see the fixation holes **260** in the mesh **270** to accommodate mechanical fixation with screws. FIG. 20B depicts a side view of the restorative **200**.

FIG. 21 depicts an embodiment having wells **265** for assisting in fixation.

FIGS. 22 and 23 depict the restorative with crimp zones **275** for localized bending.

FIG. 24 depicts a discoid shaped embodiment placed at appropriate sites on the femur; note the cut line **160** for guiding a surgeon to shape the restorative **200** for optimal fitting at appropriate sites on the femur.

FIG. 25 depicts the restorative **200** used on the iliac crest.

FIGS. 26A, 26B, and 26C depict an embodiment **200** having crimp zones **275** that guide a surgeon to forming a bowl shaped restorative **200**. FIG. 26A shows the restorative with mesh **270** side up and 26B shows the restorative **200** with foam **272** side up. FIG. 26C depicts the embodiment **200** after being guided into a bowl shape.

FIG. 27 depicts an embodiment of the present invention having a gradient of interconnectedness.

DETAILED DESCRIPTION OF PREFERRED EMBODIMENTS

In U.S. patent application Ser. No. 10/771,077, assigned to the assignee of this application and incorporated herein by reference in its entirety, there was disclosed certain graft materials for the restoration of bone, especially mammalian bone including human bone. The terms "bone graft material" and "foam" may be used interchangeably in this description. Disclosed in that application were, inter alia, biocompatible bone graft material may comprise resorbable polymer, such as collagen, and certain inorganic materials, especially calcium phosphate. The present invention provides improvements to bone graft materials by integrating mesh or other flexible support that result in the present bone restoratives. One class of these advancements that are of particular utility are pliable bone restoratives comprising an osteoconductive foam comprising biocompatible, resorbable polymer and calcium phosphate that at least partially surrounds a biocompatible mesh.

Preferably, the graft materials can be shaped or formed and are pliable. It will be appreciated that one particularly beneficial aspect of some embodiments of this invention is that it provides unprecedented utility in the surgical operatory where a reconstructive surgeon, relying upon the pliability of the bone restorative, may manipulate the restorative into shapes which are particularly amenable to the bony areas to be reconstructed. The restoratives have the capability of being fashioned into a new form and have varying degrees of pliability. It may be preferred that the restorative is deformable by human finger pressure and, when in the shape of a strip, can be rolled upon itself when wetted. Alternatively, simple hand tools such as forceps, and other common tools used in the operatory, may be employed to shape restoratives of the invention. As will readily be perceived, this enables the surgeon to tailor the precise shape of the restorative to that which is required in a particular circumstance very conveniently and at the point of use. The pliability of the restoratives of the present invention makes this possible. Relatively hard restoratives, which cannot be molded conveniently by hand or with the use of common hand tools, require extraordinary processing techniques including machinery, heat, or highly leveraged manipulative devices that are much less useful than the pliable restoratives of the present invention. Other relatively brittle bone graft materials in the art are not shapeable without crumbling.

In accordance with some embodiments of the present application, there are pliable bone restoratives comprising a biocompatible mesh at least partially surrounded by a biocompatible, resorbable polymer and the oxidation-reduction reaction product of at least one metal cation, at least one oxidizing agent, and at least one oxidizable precursor anion.

It will be appreciated that a number of alterations may be made to customize the restoratives for specific needs. There may be radiopaque embodiments. Other embodiments may be coated with titanium plasma spray to significantly increase implant surface area and mechanical retention in the bone at the time of placement. The mesh may also be acid etched titanium or sodium treated titanium to aid in mechanical interlock of the foam.

In accordance with some embodiments of the present invention, graft materials are provided wherein the resorbable polymer or polymeric material used is a collagen. Some embodiments may comprise up to 100% Type I collagen. In

other embodiments, the collagens used may be predominantly, or up to about 90%, of Type I collagen with up to about 5% of Type III collagen or up to about 5% of other types of collagen. The Type I bovine collagen may be native fibrous insoluble collagen, soluble collagen, reconstituted collagen, or combinations thereof. The biocompatible polymer may be combined with the reaction product in slurry form, or combined by blending or kneading, to form a substantially homogenous mixture. As used in this context, substantially homogenous means that the ratio of components within the mixture is the same throughout. This, upon treatment using various preferred freeze-drying and crosslinking techniques, produces a form of the present invention graft material that may be preferred.

Collagen has been found to be particularly suitable in the present invention for service as the biocompatible polymer. The admixture of the collagen with the highly porous reaction product results in a graft that is highly porous with a broad pore size distribution, increased handling properties, and pliability beyond that which is achievable with some forms of the reaction product alone, for instance calcium phosphate. The resorption profile of some of the embodiments of the present invention may vary depending upon the amount, nature, and source of the collagen or other polymer used. Typically, by twelve weeks in vivo about 80%-90% of the graft material of the present invention is resorbed. One reason that may explain the superior resorption properties of the present invention is the high degree of porosity retained even upon admixing the collagen with the reaction product. The collagen may be in a polymerized fibrous form that has a long three-dimensional architecture with multiple cross-links.

Preferable collagens have beneficial biochemical attributes such as 10% to 20% nitrogen, 10% to 15% of hydroxyproline, or up to 2.5% of ash content. In some embodiments, the collagens may be 10.5% to 17% nitrogen, 10.5% to 14% of hydroxyproline, or up to 2.5% of ash content. The percent nitrogen of a collagen is a measurement of nitrogen in a sample. In the presence of sulfuric acid, the amino nitrogen of organic material is converted to ammonium sulfate. The ammonium sulfate is distilled from an alkaline medium, and further decomposes from which the ammonia is absorbed into a boric acid solution containing a pH indicator. The ammonia (nitrogen) concentration determined colorimetrically by back titrating the boric acid solution with a standard acid.

The percent hydroxyproline of a collagen is a measure of hydroxyproline in a sample. Collagen is hydrolyzed with dilute Hydrochloric Acid, filtered and diluted. The solution is reacted with several reagents and then measured using ultraviolet (UV)/Vis analysis along with a standard hydroxyproline solution. Using the sample and standard absorbances, the percentage of hydroxyproline can be calculated $[(\text{Sample Abs})(\text{Std})(\text{Weight})(\text{dilution factor})]/[(\text{Sample weight})(\text{Std. Abs})(\text{dilution factor})]$.

The ash content of collagen is a measure of the amount of residual elements in collagen materials. When collagen is heated to extremely high temperatures, it is converted to mainly carbon dioxide and water. Elements other than collagen and hydrogen are converted to oxides and salts. A small sample of material is heated until there is only ash left. The weight of this ash is considered the gross amount of inorganic/organic material of the original sample.

Bone graft materials of this invention are held together in surgically relevant shapes and sizes by foaming the inorganic reaction product with collagen. The resulting osteoconductive foam retains substantially all of the biological and chemical properties of the shaped bodies taught in the '519 and '246 patents, while forming a shapeable, flexible unit dose. The

foam may be manufactured with the mesh into strips and cylinders of prescribed dimensions and volumes. Other shapes include but are not limited to block, hemisphere, half pipe, rod, funnel, cup, sleeve, or discoid. As seen in FIG. 8, the half pipe shaped embodiment 200 has a mesh on top of the foam portion of the restorative. The graft material portion is in contact with the metacarpal bone and the mesh is outward facing. A full pipe embodiment 200 may be seen in FIG. 9 that completely surrounds the femur. This shape may be called a bone cuff. Alternatively, the foam 272 could completely surround the mesh. The foam aids in assisting bony incorporation of the mesh and eliminates the surgical step of having to add graft material to the "structural" mesh portion of the restorative device. The foam resorbs following delivery in the surgical site and exhibit the same beneficial biological responses (e.g., bone formation) as the aforementioned shaped bodies.

The foam may be further manufactured to have a number of physical features that may assist in placing the restorative in the bony site adding support to surrounding bone. The foam may have channels 255 or wells 265 as seen in FIGS. 20A and 21. In embodiments where the mesh is embedded within the foam, these wells 265 allow a surgeon to see the mesh and the location on the mesh where a screw or suture will be fixated. The wells may also vary in size and diameter such that they are suitable for helping in the fixation of surgical screws, sutures, or wires.

Embodiments of the present invention may be described as a pliable bone restorative comprising a biocompatible mesh and a bone graft material comprising biocompatible, resorbable collagen and calcium phosphate. Other embodiments may be a pliable bone restorative comprising a biocompatible, resorbable substantially homogenous blend of a first polymeric material and a second material having interconnected macro, meso-, and microporosity, said blend at least partially surrounding a biocompatible mesh with said bone restorative. The first polymeric material may be collagen. The second material may comprise calcium phosphate.

In some embodiments, the bone graft materials may have up to about 30% by weight of biocompatible polymer. The biocompatible polymer may also be up to about 25% by weight in other embodiments. It will be appreciated that embodiments exist wherein the bone graft materials have up to about 20% or 10% by weight of a biocompatible polymer. In other embodiments where the polymer chosen is a collagen, the present invention exhibits a unique mineral (β -TCP) to collagen ratio that is unlike the ratios shared by other bone grafts. One skilled in the art may obtain bone graft materials of variable ratios depending on their particular needs. In one effective embodiment, the mass ratio of the reaction product and the collagen is 80:20. In others, it may be 90:10 or 70:30. The mass ratio may be altered without unreasonable testing using methods readily available in the art. It will be appreciated that this ratio is contrary to the mineral β -TCP to collagen ratios one skilled in the art would find in previous bone grafts while still maintaining all the properties (e.g., porosity, pore size distribution) that attribute to an effective bone graft (e.g., simultaneous bone formation, strength and graft resorption).

Due to the high porosity and broad pore size distribution (1 μ m-1000 μ m) of the graft material of the present invention, the implant is not only able to wick, soak, or imbibe materials very quickly, but is also capable of retaining them. A variety of fluids could be used with the present invention including blood, bone marrow aspirate, cell concentrate, liquid hemostat, fibrin sealant, saline, antibiotics and proteins such as bone morphogenetic proteins (BMPs).

Materials of the present invention can also be imbibed with blood, cells (e.g. fibroblasts, mesenchymal, stromal, marrow and stem cells), protein rich plasma other biological fluids and any combination of the above. This capability has utility in cell-seeding, drug delivery, and delivery of biologic molecules as well as in the application of bone tissue engineering, orthopaedics, and carriers of pharmaceuticals.

Bone restoratives of the present invention that may be preferred exhibit high degrees of porosity. It is also preferred that the porosity occur in a broad range of effective pore sizes. In this regard, persons skilled in the art will appreciate that preferred embodiments of the invention may have, at once, macroporosity, mesoporosity, and microporosity. Macroporosity is characterized by pore diameters greater than about 100 μ m and, in some embodiments, up to about 1000 μ m to 2000 μ m. Mesoporosity is characterized by pore diameters between about 100 μ m and 10 μ m, while microporosity occurs when pores have diameters below about 10 μ m. It is preferred that macro-, meso-, and microporosity occur simultaneously and are interconnected in products of the invention. It is not necessary to quantify each type of porosity to a high degree. Rather, persons skilled in the art can easily determine whether a material has each type of porosity through examination, such as through the preferred methods of mercury intrusion porosimetry, helium pycnometry and scanning electron microscopy. While it is certainly true that more than one or a few pores within the requisite size range are needed in order to characterize a sample as having a substantial degree of that particular form of porosity, no specific number or percentage is called for. Rather, a qualitative evaluation by persons skilled in the art shall be used to determine macro-, meso-, and microporosity. Therefore, some embodiments of the present invention include a pliable bone restorative comprising a biocompatible mesh and a biocompatible bone graft material comprising biocompatible, resorbable collagen and calcium phosphate having macro, meso, and microporosity.

It will be appreciated that in some embodiments of the overall porosity of materials prepared in accordance with this invention be high. This characteristic is measured by pore volume, expressed as a percentage. Zero percent pore volume refers to a fully dense material, which, perforce, has no pores at all. One hundred percent pore volume cannot meaningfully exist since the same would refer to "all pores" or air. Persons skilled in the art understand the concept of pore volume, however and can easily calculate and apply it. For example, pore volume may be determined in accordance with W. D. Kingery, *Introduction to Ceramics*, 1960 p. 416 (Wiley, 1960), who provides a formula for determination of porosity. Expressing porosity as a percentage yields pore volume. The formula is: Pore Volume=(1-f_p) 100%, where f_p is fraction of theoretical density achieved.

Porosity is measured by Helium Pycnometry. This procedure determines the density and true volume of a sample by measuring the pressure change of helium in a calibrated volume. A sample of known weight and dimensions is placed in the pycnometer, which determines density and volume. From the samples mass, the pycnometer determines true density and volume. From measured dimensions, apparent density and volume can be determined. Porosity of the sample is then calculated using (apparent volume-measured volume)/apparent volume. Porosity and pore size distribution may also be measured by mercury intrusion porosimetry.

Pore volumes in excess of about 30% may be achieved in accordance with this invention while materials having pore volumes in excess of 50% or 60% may also be routinely attainable. Some embodiments of the invention may have

pore volumes of at least about 70%. Some embodiments that may be preferred have pore volumes in excess of about 75%, with 80% being still more preferred. Pore volumes greater than about 90% are possible as are volumes greater than about 92%. In some preferred cases, such high pore volumes are attained while also attaining the presence of macro-, meso-, and microporosity as well as physical stability of the materials produced. It is believed to be a great advantage to prepare graft materials having macro-, meso-, and microporosity simultaneously with high pore volumes that also retain some compression resistance and flexibility when wetted.

In accordance with certain preferred embodiments of the present invention, a reactive blend in accordance with the invention may be imbibed into a material that is capable of absorbing it. It may be preferred that the material have significant porosity, be capable of absorbing significant amounts of the reactive blend via capillary action, and that the same be substantially inert to reaction with the blend prior to its autologous oxidation-reduction reaction. Due to this porosity, the bone graft materials disclosed herein may soak and hold fluids. As such, fluids would not be squeezed out as seen in other bone grafts found in the art. The restorative soaks and retains an approximate 1:1 volume of fluids. There are embodiments that retain over 95% soaked fluid with an applied 500 g mass. Some embodiments exhibit a wettability wherein bone graft material becomes fully saturated within 120 seconds with at least a 100% mass increase. In some embodiments, the graft material experiences a 150% mass increase and yet, in others, an approximate 200%-300% mass increase. Fluids that may be used in the present invention may be bone marrow aspirate, blood, saline, antibiotics, and proteins such as bone morphogenetic proteins (BMPs) and the like.

Wettability determines the amount of fluid taken up by sample material and if the material absorbs an appropriate amount of fluid within a specified time. Pieces of the material are randomly selected, weighed, and placed in a container of fluid for 120 seconds. If the samples adequately take up fluid, they are then weighed again to determine the percentage of mass increase from fluid absorption.

Some embodiments may be described as pliable bone restoratives comprising a biocompatible mesh and, at least partially surrounding said mesh, a biocompatible, resorbable polymer and the oxidation-reduction reaction product of at least one metal cation, at least one oxidizing agent, and at least one oxidizable precursor anion. The graft materials may be produced by methods comprising preparing an aqueous solution of a metal cation and at least one oxidizing agent. The solution is augmented with at least one soluble precursor anion oxidizable by said oxidizing agent to give rise to the precipitant oxoanion. The oxidation-reduction reaction thus contemplated is conveniently initiated by heating the solution under conditions of temperature and pressure effective to give rise to said reaction. In accordance with preferred embodiments of the invention, the oxidation-reduction reaction causes at least one gaseous product to evolve and the desired intermediate precursor mineral to precipitate from the solution.

The intermediate precursor mineral thus prepared can either be used "as is" or can be treated in a number of ways. Thus, it may be heat-treated greater than about 800° C. or, preferably, greater than about 1100° C. in accordance with one or more paradigms to give rise to a preselected crystal structure or other preselected morphological structures therein. In accordance with preferred embodiments, the oxidizing agent is nitrate ion and the gaseous product is a nitrogen oxide, generically depicted as $\text{NO}_{x(g)}$. It is preferred that

the precursor mineral provided by the present methods be substantially homogenous. As used in this context, substantially homogenous means that the porosity and pore size distribution throughout the precursor mineral is the same throughout.

In accordance with other preferred embodiments, the intermediate precursor mineral provided by the present invention may be any calcium salt. Subsequent modest heat treatments convert the intermediate material to e.g. novel monophasic calcium phosphate minerals or novel biphasic β -tricalcium phosphate (β -TCP)+type-B, carbonated apatite (c-HAp) [$\beta\text{-Ca}_3(\text{PO}_4)_2 + \text{Ca}_5(\text{PO}_4)_{3-x}(\text{CO}_3)_x(\text{OH})$] particulates. More preferably, the heat treatment converts the intermediate material to a predominantly β -TCP material.

It will be appreciated that the porosity is similar to that of inorganic shaped bodies disclosed in the '519 and '246 patents. The bone graft materials of the present invention are indeed improvements on the shaped bodies disclosed in the '519 and '246 patents. For some embodiments of the present invention, the shaped bodies of the '519 and '246 patents are modified using various natural and synthetic polymers, film forming materials, resins, slurries, aqueous mixtures, pre-polymers, organic materials, metals, and other adjuvants. Materials such as collagen, wax, glycerin, gelatin, polycaprolactone, pre-polymeric materials such as precursors to various nylons, acrylics, epoxies, polyalkylenes, and the like, were caused to permeate all or part of the shaped bodies formed in accordance with the '519 and '246 patents. The soak and hold properties of some graft materials disclosed herein exhibit at least a greater than 100% mass increase of blood. Many of the bone restoratives have a tough structural integrity with improved clinical handling when compared to the bodies of the '519 and '246 patents.

An embodiment of the present invention includes pliable restoratives for the restoration of bone in the form of a shaped body, the shaped body selected to conform generally to a mammalian, anatomical tissue structure, said body comprising a polymer and beta tricalcium phosphate, and partially surrounding a biocompatible mesh; the graft having interconnected macro-, meso-, and microporosity.

The bone restoratives have improved handling that can provide a unit dose delivery. The addition of a polymer in the graft material greatly enhances the ability of the product to be shaped or cut without crumbling. The restoratives may be shaped or cut using various instruments. This feature finds utility in a variety of surgical applications, particularly since the bone graft can be formed "in situ" in an operating room to suit the needs of the patient in cases where the bone void to be filled is an irregular shape. Some restoratives disclosed may also be delivered into the bony site directly, shaped, and allowed to wick bodily fluids by an operator while during an operation.

It will be appreciated that the handling ability of the restoratives will fall under a number of descriptions. The restoratives may be described as being very pliable, malleable, or even formable. As used herein, pliable means supple enough to bend freely without breaking. In the context of the present application, malleable means capable of being altered or controlled by outside forces or influence. As used herein, formable means to become formed or shaped. It can also be said that the restoratives have high ductility, which means easily molded or shaped in the present context. A surgeon using one of the embodiments of the present invention should be able to shape and form the restorative using the force of his hands or fingers.

The bone graft materials may be sterilized and may be preferably gamma irradiated at a range of about 25 kGy to 40 kGy.

Many of the embodiments disclosed herein are to fill bony voids and defects and may not be intrinsic to the stability of the surgical site. It will be appreciated that applications for the embodiments of the present invention include, but are not limited to, filling interbody fusion devices or cages (ring cages, cylindrical cages), placement adjacent to cages (i.e., in front cages), placement in the posterolateral gutters in posteriolateral fusion (PLF) procedures, backfilling the iliac crest, acetabular reconstruction and revision hips and knees, large tumor voids, use in high tibial osteotomy, burr hole filling, and use in other cranial defects. Bone restorative strips may be suited for use in PLF by placement in the posterolateral gutters, and in onlay fusion grafting. Additional uses may include craniofacial and trauma procedures that require covering or wrapping of the injured/void site. The bone restorative cylinders may be suited to fill spinal cages and large bone voids, and for placement along the posterolateral gutters in the spine.

Due to the wide range of applications for the embodiments of the present invention, it should be understood that the present invention restoratives could be made in a wide variety of shapes and sizes via standard molding techniques. For instance, blocks and cylinders of the present invention may find utility in bone void filling and filling of interbody fusion devices; wedge shaped devices of the present invention may find utility in high tibial osteotomies; and strips may find utility in cranial defect repairs. In general, the bone restoratives will take a variety of forms including cylindrical, block, or discoid shapes. Of particular interest, may be the use of some of the restoratives as semi-spherical (FIG. 3A), semi-tubular (FIGS. 7A-7C) or disc-shaped (FIG. 4A) strips for containment devices. An embodiment of the semi-spherical form **102** in use is depicted in FIG. 3B. Some embodiments are ring shaped with the mesh being partially surrounded by the graft material. The graft material may also be surrounded by the mesh in this embodiment.

It will be appreciated that these shapes are not intended to limit the scope of the invention as modifications to these shapes may occur to fulfill the needs of one skilled in the art. The benefits of the restoratives that, for instance, may be used in acetabular reconstruction made from the present invention are several-fold. The restorative may act as both a barrier to prevent migration of other implants and serves to promote bone formation. The bone restorative device may be relatively non-load bearing, or partially load bearing, or may be reinforced to be fully load bearing as described below. Depending on the form, the restoratives have barrier properties because it maintains its structural integrity.

In applications requiring graft materials with partial load bearing capabilities, the graft materials of the present invention may have meshes or plates affixed. The meshes or plates may be of metal, such as titanium or stainless steel, or of a polymer or composite polymer such as polyetheretherketone (PEEK), or nitinol. As depicted in FIGS. 6A and 6B, a metallic mesh **270** may be placed to one side of the bone graft material **272** to add strength and load bearing properties to the implant. In FIG. 6A, the mesh plate **270** sits affixed to one surface of the graft material **272**. In FIG. 6B, the mesh plate **270** penetrates one surface of the graft material **272** with one side of mesh exposed on top. In FIG. 6C, the mesh plate **270** is immersed more deeply than in FIG. 6B within the graft material **272**. FIGS. 7A-7C depict another embodiment of the restorative **200** in semi-tubular form. A mesh may be affixed to a surface for further support in long bone reinforcement or

may be completely surrounded by the osteoconductive foam. Due to the unique properties of the present invention graft material, the mesh may be affixed in the body using sutures, staples, screws, cerclage wire or the like.

One skilled in the art may place the mesh in any location necessary for a selected procedure in a selected bodily void. For instance, a composite of mesh and graft material could be used in a craniomaxillofacial skull defect with the more pliable graft surface being placed in closer proximity to the brain and the more resilient mesh surface mating with the resilient cortical bone of the skull. In this manner, the mesh or plate may be affixed to one side of the graft material. Alternatively, the mesh or plate may be affixed to both sides of the graft material in sandwich fashion. Likewise, graft material could be affixed to both sides of the mesh or plate. The mesh may exist in non-congruent fashion throughout the graft material. In other words, the mesh may be selectively positioned throughout the graft material. The meshes may be flat or may be shaped to outline the graft material such as in a semi-spherical, semi-tubular, or custom form. These embodiments may be unique due to their integral relation between the graft material and the mesh. This is contrary to other products in the field in which the graft material is placed adjacent to the structural implant or, in the case of a cage, within the implant.

In accordance with the present invention, another embodiment provides a bone graft for long bone reinforcement comprising a biocompatible, resorbable semi-tubular shape, or sleeve, of a polymer and beta-tricalcium phosphate, the graft having interconnected macro-, meso-, and microporosity. A mesh may be affixed to the surface of the sleeve or may be immersed in the sleeve. The mesh may be made of titanium, stainless steel, nitinol, a composite polymer, or polyetheretherketone. In some embodiments that may be preferred, the polymer may be collagen. The beta-tricalcium phosphate and polymer may be in a mass ratio of about 90:10 to about 70:10, or about 85:15 to about 75:25. The cross-section of the sleeve may be in the shape of a crescent shape moon (FIG. 7B).

The mesh may also comprise crimped areas for localized bending or shaping as shown in FIG. 22. This crimp line may also guide a surgeon in cutting the restorative before placing it on bone. These zones assist an operator in manipulating the restorative into predetermined shapes. For instance, as shown in FIG. 22, the disc is crimped or scored in concentric circles so that an operator will be guided to bend the disc to make a cup. As shown in FIG. 27, the foam portion of the bone restorative may exhibit a gradient of interconnectedness with tuneable properties. This embodiment is one in which restorative exhibits a designated porosity in one area of the bone restorative and the porosity gradually changes towards another area of the restorative. For instance, the gradient may represent an integration of materials and properties such that the left-most portion of the restorative is comprised of a first relatively dense material with a first porosity (p_1), the left middle portion of the restorative is the same first relatively dense material but with a second porosity (p_2), the right middle portion of the restorative is a second relatively porous material with a third porosity (p_3), and the right-most portion of the restorative is the same second relatively porous material but with a fourth porosity (p_4), wherein $p_4 > p_3 > p_2 > p_1$, which creates the gradient. In other embodiments, there is a stiffness gradient that is a measure of load bearing capabilities that gradually increases or decreases from one portion of the restorative to the other portion of the restorative. In order to have such a porosity, stiffness, or load-bearing gradient, the materials and their properties, such as porosity, to be integrated may vary. That is, the first material of the bone restorative may be comprised of a metal, polylactic acid, carbon-

fiber reinforced composite, collagen, or mesh that is integrated as described above with the second material calcium phosphate, bone graft materials, bone graft substitutes or porous resorbable structures. In other embodiments, the gradient could be one of both porosity and stiffness. In this manner, the type of material, the thickness of the material, and the porosity all play a role.

The mesh material may also exhibit variable porosity. The entire mesh material in some embodiments will be uniform throughout. In some embodiments, the porosity of the device will be from about 30% to about 95%. However, it will be appreciated that some embodiments may have meshes having multiple zones of porosity and thickness. A lower degree of porosity may be needed in an area of the restorative where that area will be used for load bearing applications. In non-load bearing zones, the restorative may have increased mesh porosity. The mesh, on some embodiments with have a thickness between about 0.1 mm to about 2.5 mm. In other embodiments that may be preferred, the thickness can be about 0.5 mm. The thickness of the mesh may be equal throughout or may vary as with porosity such that it is thicker in areas requiring load-bearing capabilities and thinner in non-load bearing zones. Total device thickness may be from about 1 mm to about 4 cm. In some embodiments that may be preferred, the total thickness may be 4 mm.

The surface texture of the mesh may also vary depending on the need and depending upon the degree of adhesion that is required between the mesh and the foam to be integrated. The surface texture may be measured by a roughness measurement. It will be appreciated that in some embodiments, the roughness measurement will be high like that of sandpaper. In other embodiments, the mesh may have a low roughness measurement like that of a sheet of ice. It is foreseeable that one skilled in the art will vary the surface texture to fit their particular need.

The graft materials can also be imbibed with any bioabsorbable polymer or film-forming agent such as polycaprolactones (PCL), polyglycolic acid (PGA), poly-L-Lactic acid (PL-LA), polysulfones, polyolefins, polyvinyl alcohol (PVA), polyalkenoics, polyacrylic acids (PAA), polyesters and the like. The resultant graft material is strong, carveable, and compressible. The grafts of the present invention coated with agents such as the aforementioned may still absorb blood.

In another embodiment of the present invention, the bone restoratives may be used as an attachment or coating to any orthopaedic implant such as a metal hip stem, acetabular component, humeral or metatarsal implant, vertebral body replacement device, pedicle screw, general fixation screw, plate or the like. The coating may be formed by dipping or suspending the implant for a period of time in a substantially homogenous slurry of polymer and mineral and then processing via freeze-drying/lyophilization and crosslinking techniques. As used in this context, substantially homogenous means that the ratio of elements within the slurry is the same throughout. Alternatively, a female mold may be made of the implant and the slurry may be poured into the mold and processed, as described above, to form the coating.

It will be appreciated that methods of treating bony defects are foreseen by the embodiments of the present invention. A method for restoring or repairing bone in an animal comprising accessing a site to be restored; and implanting into a bony space a bone graft material comprising biocompatible, resorbable collagen, the oxidation-reduction reaction product of at least one metal cation, at least one oxidizing agent, and at least one oxidizable precursor anion. The graft material used in this method may be chosen by one skilled among those disclosed in the present application.

EXAMPLES

Example 1

One embodiment was comprised of β -TCP, with a cation to anion ratio of $\text{Ca}_3(\text{PO}_4)_2$; and medical grade Type I bovine collagen, manufactured in the following manner. Inorganic scaffolds were made using the RPR process disclosed in U.S. Pat. Nos. 5,939,039 and 6,325,987. The resultant inorganic scaffolds were crushed and sieved to obtain morsels in the size range of 0.25 mm-4 mm. The morsels were added to a fibrous collagen slurry in a wet processing room and the resultant slurry was further mixed and casted/molded into various shapes in a cleanroom. The shapes were freeze-dried and crosslinked using dehydrothermal (DHT) treatment to produce resultant bone graft material shaped products.

Example 2

Mineral Component of Bone Graft Material

Approximately 78%-82% by weight of some bone graft materials of the present invention is β -TCP, with the cation to anion ratio of $\text{Ca}_3(\text{PO}_4)_2$. Each lot of the mineral component of these bone graft materials was tested using X-ray diffraction (XRD) to confirm phase pure β -TCP in accordance with ASTM F1088-87, Standard Specification for Beta-Tricalcium Phosphate for Surgical Implantation. In addition to XRD, Inductively Coupled Plasma Chromatography (ICP) was used to demonstrate that the levels of heavy metals in the predicate bone graft material are below those established in ASTM F-1088-87. Fourier Transform Infrared Spectroscopy (FTIR) analyses of the bone graft material were also performed.

The quantitative XRD results show that the mineral component of the bone graft material is 98.25% pure β -TCP, which matches well with the ICDS standard plot for β -TCP pictured with the representative XRD pattern of the bone graft material (FIG. 11). The ICP results for the bone graft material show that the levels of heavy metal contaminants—arsenic (As), cadmium (Cd), mercury (Hg), and lead (Pb), are below the method detection limits of 2.25 ppm, 1.80 ppm, 2.25 ppm and 4.5 ppm, respectively, thus below the limits set forth in ASTM F-1088-87. Qualitative FTIR results show a 95% match of the bone graft material to greater than 99% pure β -TCP. A representative FTIR spectrum is shown in FIG. 12.

Example 3

Bulk Density

Bulk density of bone graft material was calculated from three representative samples. Each sample was measured in triplicate to provide an average calculated density of 0.46 g/cc \pm 0.03 g/cc.

Example 4

Porosity and Pore Size Distribution

In one embodiment of the present invention, as determined by mercury intrusion porosimetry, pore diameters in the graft range from 1 μm to 1000 μm . Approximately 5% to 15% of the pores are greater than 100 μm , approximately 50%-70% of the pores are between 10 μm -1100 μm , and approximately 20%-35% of the pores are less than 10 μm . The larger macro pores (greater than 100 μm) allow bone to grow in apposition to the calcium phosphate surfaces of the implant. The smaller

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meso (10 μm -100 μm) and micro (less than 10 μm) interconnected pores allow for fluid communication and nutrient transport. Total porosity is approximately 70%-80%.

Example 5

Scanning Electron Microscopy Evaluation

Scanning electron micrographs (SEM) of one embodiment of the present invention graft material are provided in FIGS. 13, 14, and 15.

Example 6

In-Vivo

A GLP animal study was performed at North American Science Associates, Inc. (NAMSA), Northwood, Ohio, to evaluate the biological effects of the bone graft material and a control in metaphyseal defects of adult dogs. Sixteen dogs were implanted both with one embodiment of the present invention and the control. Animals were sacrificed at each of the time periods of 3, 6, 12, and 24 weeks. Gross evaluation, radiographic assessment, histological evaluation, histomorphometry, and mechanical evaluations were performed.

In this animal study, the control was placed in the proximal humerus, and the present invention was placed in the femoral condyle.

Quantitative Histology

Qualitatively, by 12 weeks approximately 80%-90% of the bone graft material implant was resorbed and the amount of new bone in the implant was approximately 20%-25%. For the predicate (control) at 12 weeks, approximately 80%-90% of the implant was resorbed and the amount of new bone in the implant was approximately 30%-35%. By 24 weeks, the estimated amount of new bone in the implant was approximately 25-35% for both, with equivalent resorption of each material.

Mechanical Evaluation

In addition to histology, half of each specimen from the animal study was utilized for biomechanical indentation testing. In brief, a flat-head indenter with a diameter equal to half the diameter of the defect (e.g., 5 mm diameter indenter for mm humeral defects and 4 mm diameter indenter for 8 mm femoral condyle defects) was lowered (compression) into the center of the defect in order to evaluate the structural properties of the repaired defect at 3, 6, 12, and 24-week time points. For comparison purposes, the indenter was also lowered in an area adjacent to the defect to evaluate the structural properties of the adjacent bone. Ultimate indentation load, yield load, stiffness, and ultimate indentation strength were quantified.

By twelve weeks, strength between the bone graft material and control was similar, and not significantly different. In addition, the strength and stiffness of each material at this time point were statistically similar to the respective adjacent bone.

The similarities in strength and stiffness between the bone graft material repaired defect site and the control repaired defect site are readily apparent after normalization with the adjacent bone.

Example 7

Gelatin Modification

A piece of the inorganic material was immersed in a solution prepared by dissolving 7.1 g food-grade gelatin (CAS #9000-70-0) (Knox Unflavored Gelatin, Nabisco Inc., East

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Hanover, N.J. 07936) in 100.0 g deionized water at approximately 90° C. The inorganic material readily imbibed the warm gelatin solution and, after several minutes, the largely intact piece of inorganic material was carefully removed from the solution and allowed to cool and dry overnight at room temperature. The gelatin solution gelled on cooling and imparted additional strength and improved handling properties to the inorganic material. Although no pH or electrolyte/nonelectrolyte concentration adjustments were made to the system described in this example, it is anticipated that such adjustments away from the isoelectric point of the gelatin would impart additional rigidity to the gelatin gel and, thereby, to the gelatin-treated inorganic material. Significant additional strength and improved handling properties were noted in the gelatin-treated inorganic material after the gelatin was allowed to thoroughly dry for several days at room temperature. Some shrinkage of the gelatin-treated inorganic materials was noted on drying. The shrinkage was nonuniform with the greatest contraction noted near the center of the body. This central region was, of course, the last area to dry and, as such, was surrounded by hardened inorganic material which could not readily conform to the contraction of the core as it dehydrated. The material exhibited considerable improvement in compression strength and a dramatically reduced tendency to shed particulate debris when cut with a knife or fine-toothed saw. It is presumed that the film-forming tendency of the gelatin on drying induced compressive forces on the internal cellular elements of the inorganic sponge material, thereby strengthening the overall structure.

Cylindrical plugs could be cored from pieces of the air dried gelatin-treated inorganic material using hollow punch tools ranging from 1/2 inch down to 1/8 inch in diameter.

FIG. 17 is a SEM of the air-dried gelatin treated inorganic material. FIG. 18 is a SEM of sheep trabecular bone. The highly porous macrostructure of sheep trabecular bone is representative of the anatomical structure of cancellous bone of higher mammals, including humans. The sample of sheep trabecular bone was prepared for SEM analysis by sputter coating a cross-sectional cut from a desiccated sheep humerus. FIG. 19 is a higher magnification SEM of the air-dried gelatin treated inorganic material depicted in FIG. 17. From this SEM micrograph, the presence of meso- and microporosity in the calcium phosphate matrix is readily apparent.

Example 8

Sterilization

Samples of gelatin-treated inorganic material were prepared as described in Example 7 and allowed to thoroughly dry at room temperature for longer than one week. Pieces of this dry gelatin-treated material were subjected to prolonged oven treatment in an air atmosphere within a Vulcan model 3-550 oven to simulate conditions typically encountered in "dry heat" sterilization procedures. The following table summarizes these experiments

Temperature (° C.)	Time (h)	Observations
130	3	No color change
130	6	Very slight yellowing
130	15	Very slight yellowing
150	4	Very slight yellowing
170	1	Very slight yellowing
170	3.5	Pale yellow at surface, white interior

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It was assumed that temperature equilibration between the samples and the oven was rapidly attained due to the significant porosity and low thermal mass of the materials. Clearly, there was no significant degradation of the gelatin under these heat treatments regimens. Furthermore, a subjective assessment of the strength of these dry heat treated specimens showed no apparent changes.

Example 9

Template Residues

A reactant solution was prepared as described in the '162 patent. A variety of shapes, including disks, squares, and triangles, were cut from a sheet of $\frac{3}{32}$ inch thick sponge material (Spontex, Inc., P.O. Box 561, Santa Fe Pike, Columbia, Term. 38402) using either scissors or hollow punches. The cut pieces of compressed sponge were fully imbibed with the reactant solution after which they swelled to form cylinders, cubes, and wedges. These solution saturated sponge articles were placed into an oven preheated to 500° C. and held at that temperature for 1 hour. After cooling, the inorganic sponge pieces were carefully removed from the considerable amount of crusty white solid resulting from the exudate material. All samples had been converted to an inorganic replica of the original organic sponge structures. The vestigial structures represented positive versions of the original sponge structures with faithful replication of the cellular elements and porosity. The vestigial masses were fragile with very low apparent density, but they were robust enough to be handled as coherent blocks of highly porous solid once they were removed from the exudate material. After refring the samples between 800° C. to 1100° C. (Vulcan furnace) for 15 minutes, the final inorganic sponge samples were completely white. The integrity of the various samples made from the controlled porosity cellulose sponge was improved over corresponding samples prepared from the commercial cellulose sponge materials. The samples were then crushed and sieved to obtain morsels in the size range of 0.25 mm-4 mm. The morsels were added to a collagen slurry in a wet processing room and the resultant slurry was further mixed and casted/molded into various shapes in a cleanroom. The shapes were freeze-dried and crosslinked to produce resultant bone graft material shaped products.

Example 10

Modified Templates

Pieces of an inorganic sponge material were immersed in a gelatin solution prepared as described in Example 7 except that 7.1 g of Knox gelatin was dissolved in 200 g deionized water rather than 100 g of deionized water. The inorganic sponge material readily imbibed the warm gelatin solution and, after several minutes, the largely intact pieces of inorganic sponge material were carefully removed from the solution and allowed to cool and dry at room temperature. Significant additional strength and improved handling properties were noted in the gelatin-treated inorganic sponge material after the gelatin was allowed to thoroughly dry for several days. The material exhibited considerable improvement in compression strength and a dramatically reduced tendency to shed particulate debris when cut with a knife or fine-toothed saw. Several pieces of gelatin treated sponge which had been drying in air for over 1 week were subjected to a burnout of the organic material at 800° C. (Vulcan furnace) for 30 minutes. The snow white inorganic sponge samples were weighed

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after firing and it was determined that the level of gelatin in the treated samples was 13.8 ± 1.0 wt % (with respect to the inorganic sponge material).

Example 11

Rewetting

Several pieces of air-dried gelatin-treated inorganic sponge material from Example 7 were placed in deionized water to assess the rewetting/rehydration behavior. Initially, the pieces floated at the water surface but, after approximately 2 hours, the sponge pieces began to float lower in the water indicating liquid uptake. After 24 hours, the samples were still floating, but greater than 50% of the sponge volume was below the liquid surface. After 48 hours, the inorganic sponge samples were completely submerged suggesting complete rehydration of the gelatin and complete water ingress into the structure via interconnected porosity.

Example 12

Shaped Calcium Phosphates

Several pieces of the inorganic sponge material made from U.S. Pat. Nos. 5,939,039 and 6,325,987 were immersed in a 50 wt % solution of disodium glycerophosphate hydrate in 10.0 g deionized water. The inorganic sponge material readily imbibed the disodium glycerophosphate solution and, after several minutes, the largely intact pieces of saturated inorganic sponge material were carefully removed from the solution. The wetted pieces were placed in a Vulcan model 3-550 oven preheated to 150° C. Immediately, temperature was ramped to 850° C. followed by a 60 minute hold. After cooling to room temperature, the surface of the treated inorganic sponge material had a glassy appearance, and significant additional strength and improved handling properties were noted. Upon examination of the pieces with a Leica™ zoom stereo microscope, the presence of a glassy surface was confirmed and rounding of the features was evident indicating that some level of sintering had occurred. Considerable shrinkage of the pieces was also noted.

Example 13

Discoïd Bodies

A reactant solution was prepared as described in the '519 patent. Disks were cut from a sheet of $\frac{3}{32}$ inch thick compressed sponge using a $\frac{3}{8}$ inch diameter hollow punch and a model No. 3393 Carver hydraulic press (Carver Inc., 1569 Morris St., P.O. Box 544, Wabash, Ind. 46992) to ensure uniform sizing. The disks were distended by immersion in deionized water and the resulting sponge cylinders, each approximately $\frac{3}{8}$ inch diameter by 1 inch length, were then blotted on paper towel to remove as much excess water as possible. The damp sponge cylinders were then imbibed with approximately seven times their weight of the reactant liquid. Nine of the solution imbibed pieces were placed horizontally and spaced uniformly in a 100mm×20mm Pyrex petri dish. Two petri dishes, containing a total of 18 imbibed sponge cylinders, were irradiated for a total of two minutes. After 30 seconds of exposure, the reactant liquid, which had exuded from the sponge cylinders, had reacted/dehydrated to form a crusty white deposit in the petri dishes. After several additional cycles of exposure, the fully dried sponge cylinders were removed. The dried, solid-filled cylindrical sponge pieces were arrayed in a rectangular alumina crucible ($2\frac{1}{2}$ "

W×6" L×½" D) and placed in a furnace preheated to 500° C. The furnace temperature was ramped at 40° C./minute to 800° C. and held at 800° C. for 45 minutes. The resultant cylindrical white porous inorganic sponge samples were robust and exhibited strengths qualitatively similar to those attained from the fully dried gelatin-treated samples prepared as described in Example 10.

Example 14

Bone Wrap and Universal Plate

A 100 mm×100 mm square mesh was formed. The foam portion had a thickness of 3 mm to 3.5 mm and the mesh portion had a thickness of 0.5 mm to 1 mm. Ovoid shaped holes were made in the thin, malleable mesh. The bone restorative, mesh plus foam, had a total thickness of 4 mm. The mesh was then embedded in the foam portion.

A 50 mm×100 mm mesh was formed. The approximate thickness of the foam portion was about 3 mm thick. A mesh shaped foam portion was formed having the characteristic variety of pore sizes. A slightly malleable mesh having about 1 mm thickness was formed and placed on top portion of the foam. Screw holes to accommodate standard titanium trauma screws were formed extending through the bone restorative.

What is claimed is:

1. A pliable bone restorative comprising:
 - a biocompatible mesh; and,
 - a pliable bone graft material comprising a homogeneous composite of biocompatible, resorbable polymer and biocompatible, resorbable calcium phosphate; wherein said bone graft material has macro-, and microporosity and at least partially surrounds said mesh; and,
 - wherein said bone restorative is wetted with a fluid.
2. The bone restorative of claim 1 wherein said polymer is collagen.
3. The bone restorative of claim 1 wherein said fluid comprises bone marrow aspirate, cell concentrate, liquid hemostat, fibrin sealant, blood, saline or any combination thereof.
4. The bone restorative of claim 1 having a cylindrical, block, wedge, sheet, hemisphere, half pipe, rod, funnel, or discoid shape.
5. The bone restorative of claim 1 wherein said mesh comprises titanium, stainless steel, nitinol, a composite polymer, or polyetheretherketone.
6. The bone restorative of claim 5 wherein said mesh comprises acid etched titanium or sodium treated titanium.
7. The bone restorative of claim 1 wherein said restorative is coated with titanium plasma spray.
8. The bone restorative of claim 1 that is radiopaque.
9. The bone restorative of claim 1 wherein said bone graft material completely surrounds said mesh.
10. A pliable bone restorative comprising:
 - a biocompatible mesh; and,
 - a pliable bone graft material comprising a homogeneous composite of biocompatible, resorbable polymer, and the biocompatible, resorbable oxidation-reduction reaction product of at least one metal cation, at least one oxidizing agent, and at least one oxidizable precursor anion,
 - wherein said bone graft material has macro-, meso-, and microporosity and at least partially surrounds said mesh, and,
 - wherein said bone restorative is wetted with a fluid.
11. The bone restorative of claim 10 wherein said polymer is collagen.

12. The bone restorative of claim 10 wherein said a fluid comprising bone marrow aspirate, cell concentrate, liquid hemostat, fibrin sealant, blood, saline or any combination thereof.

13. The bone restorative of claim 10 having a cylindrical, block, wedge, sheet, hemisphere, half pipe, rod, funnel, or discoid shape.

14. The bone restorative of claim 10 wherein said mesh comprises titanium, stainless steel, nitinol, a composite polymer, or polyetheretherketone.

15. The bone restorative of claim 14 wherein said mesh comprises acid etched titanium or sodium treated titanium.

16. The bone restorative of claim 10 wherein said restorative is coated with titanium plasma spray.

17. The bone restorative of claim 10 that is radiopaque.

18. A pliable bone restorative comprising:

- a biocompatible mesh; and
- a pliable bone graft material comprising a homogeneous composite of biocompatible, resorbable collagen and biocompatible, resorbable calcium phosphate, wherein said bone graft material has macro-, meso-, and microporosity,

wherein said bone restorative is wetted with a fluid and wherein at least a portion of the biocompatible mesh is in contact with the bone graft material.

19. The bone restorative of claim 18 wherein said fluid comprises bone marrow aspirate, cell concentrate, liquid hemostat, fibrin sealant, blood, saline or any combination thereof.

20. The bone restorative of claim 18 having a cylindrical, block, wedge, sheet, hemisphere, half pipe, rod, funnel, or discoid shape.

21. The bone restorative of claim 18 wherein said mesh comprises titanium, stainless steel, nitinol, a composite polymer, or polyetheretherketone.

22. The bone restorative of claim 21 wherein said mesh comprises acid etched titanium or sodium treated titanium.

23. The bone restorative of claim 18 wherein said restorative is coated with titanium plasma spray.

24. The bone restorative of claim 18 that is radiopaque.

25. A pliable bone restorative comprising:

- a biocompatible mesh; and
- a pliable, biocompatible bone graft material comprising a homogeneous composite of biocompatible, resorbable collagen and biocompatible, resorbable calcium phosphate having macro, meso, and microporosity,

 wherein said bone restorative is wetted with a fluid and wherein at least a portion of the biocompatible mesh is in contact with the bone graft material.

26. The bone restorative of claim 25 wherein said fluid comprising bone marrow aspirate, cell concentrate, liquid hemostat, fibrin sealant, blood, saline or any combination thereof.

27. The bone restorative of claim 25 having a cylindrical, block, wedge, sheet, hemisphere, half pipe, rod, funnel, or discoid shape.

28. The bone restorative of claim 25 wherein said mesh comprises titanium, stainless steel, nitinol, a composite polymer, or polyetheretherketone.

29. The bone restorative of claim 28 wherein said mesh comprises acid etched titanium or sodium treated titanium.

30. The bone restorative of claim 25 wherein said restorative is coated with titanium plasma spray.

31. The bone restorative of claim 25 that is radiopaque.

32. A pliable bone restorative comprising:

- a biocompatible mesh; and,

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a pliable, biocompatible, resorbable homogeneous blend of a first polymeric material and a second biocompatible, resorbable material comprising the oxidation-reduction product of at least one metal cation, at least one oxidizing agent, and at least one oxidizable precursor anion and having interconnected macro, meso-, and microporosity,

wherein said blend at least partially surrounds said biocompatible mesh, and wherein said bone restorative is wetted with a fluid.

33. The bone restorative of claim 32 wherein said polymeric material is collagen.

34. The bone restorative of claim 32 wherein said second material comprises calcium phosphate.

35. The bone restorative of claim 32 wherein said fluid comprises bone marrow aspirate, cell concentrate, liquid hemostat, fibrin sealant, blood, saline, or any combination thereof.

36. The bone restorative of claim 32 having a cylindrical, block, wedge, sheet, hemisphere, half pipe, rod, funnel, or discoid shape.

37. The bone restorative of claim 32 wherein said mesh comprises titanium, stainless steel, nitinol, a composite polymer, or polyetheretherketone.

38. The bone restorative of claim 37 wherein said mesh comprises acid etched titanium or sodium treated titanium.

39. The bone restorative of claim 32 wherein said restorative is coated with titanium plasma spray.

40. The bone restorative of claim 32 that is radiopaque.

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41. A pliable bone restorative for the restoration of bone in the form of a shaped body, the shaped body selected to conform generally to a mammalian, anatomical tissue structure, said body comprising:

5 a biocompatible mesh; and,

a pliable bone graft material comprising a homogeneous composite of polymer and biocompatible, resorbable beta tricalcium phosphate having interconnected macro-, meso-, and microporosity;

10 wherein said bone graft material at least partially surrounds said mesh, and wherein said bone restorative is wetted with a fluid.

42. The bone restorative of claim 41 wherein said polymer comprises collagen.

15 43. The bone restorative of claim 41 having a cylindrical, block, wedge, sheet, hemisphere, half pipe, rod, funnel, or discoid shape.

20 44. The bone restorative of claim 41 wherein said fluid comprises bone marrow aspirate, cell concentrate, liquid hemostat, fibrin sealant, blood, saline, or any combination thereof.

45. The bone restorative of claim 41 wherein said mesh comprises titanium, stainless steel, nitinol, a composite polymer, or polyetheretherketone.

25 46. The bone restorative of claim 45 wherein said mesh comprises acid etched titanium or sodium treated titanium.

47. The bone restorative of claim 41 wherein said restorative is coated with titanium plasma spray.

48. The bone restorative of claim 41 that is radiopaque.

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